

# CellML modularity and the Physiome Model Repository

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NEW ZEALAND

Te Whare Wānanga o Tāmaki Makaurau

# Outline

- Introduction to CellML
- Modularity in CellML
- The Physiome [CellML] model repository
- PMR2 – the software behind the repository
- Multiscale modelling



a quick introduction...

# What is CellML?

CellML is an XML-based markup language used to describe mathematical models of biological processes

- Equations are expressed in MathML, and metadata are expressed in RDF
- But why is there a need for CellML?

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<component name="membrane">
  <variable units="millivolt" public_interface="out"
  cmeta:id="membrane_V" name="V" initial_value="-86.2" />
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  name="R" initial_value="8314.472" />
  <variable units="kelvin" public_interface="out" name="T"
  initial_value="310" />
  <variable units="coulomb_per_millimole" public_interface="out"
  name="F" initial_value="96485.3415" />
  <variable units="microF" public_interface="out" name="Cm"
  initial_value="0.185" />
  <variable units="micrometre3" public_interface="out" name="V_c"
  initial_value="0.016404" />

  <variable units="millisecond" public_interface="in"
  name="time" />
  <variable units="picoA_per_picoF" public_interface="in"
  name="i_K1" />
  <variable units="picoA_per_picoF" public_interface="in"
  name="i_to" />
  <variable units="picoA_per_picoF" public_interface="in"
  name="i_Kr" />
  <variable units="picoA_per_picoF" public_interface="in"
  name="i_Ks" />
  <variable units="picoA_per_picoF" public_interface="in"
  name="i_CaL" />
  <variable units="picoA_per_picoF" public_interface="in"
  name="i_NaK" />
  <variable units="picoA_per_picoF" public_interface="in"
  name="i_p_K" />

  <math xmlns="http://www.w3.org/1998/Math/MathML">
    <apply><eq />
      <apply><diff />
        <bvar><ci>time</ci></bvar>
        <ci>V</ci>
      </apply>
      <apply><times />
        <apply><divide />
          <apply><minus />
            <cn cellml:units="dimensionless">1</cn>
          </apply>
          <cn cellml:units="dimensionless">1</cn>
        </apply>
        <apply><plus /><ci>i_K1</ci>
          <ci>i_to</ci><ci>i_Kr</ci>
          <ci>i_Ks</ci><ci>i_CaL</ci>
          <ci>i_NaK</ci><ci>i_Na</ci>
          <ci>i_b_Na</ci><ci>i_NaCa</ci>
          <ci>i_b_Ca</ci><ci>i_p_K</ci>
          <ci>i_p_Ca</ci><ci>i_Stim</ci>
        </apply>
      </apply>
    </math>
  </component>

```

model creation

```

%-----Calc the L-type Ca current-----
      [CfCa,RevPCa]=
CalcConstantfield(Cai,Cao,2, Vm); %Ca
      [CfK,RevPK] = CalcConstantfield(Ki,Ko,1,
Vm); %K
      [CfNa,RevPNa] =
CalcConstantfield(Nai,Nao,1, Vm); %Na
      if (count ==1 && currenttime == 0)
          Va = -74.0078;
      else
          Va = Vm;
      end
      if (count ==0)
          [mcal, hcal,n] =
calcRateConst(1,Va,0,Cai,mcal,hcal,count,dt); %Calc
m and h
          ICaLNa =
(0.00005*PCAL*CfNa)*mcal*hcal;
          ICaLK = (0.001 * PCAL * CfK)*mcal*hcal;
          %ICaLCa = (PCAL * CfCa*mcal*hcal);
%original
          ICaLCa = (PCAL * CfCa*mcal*hcal);
          ICaL = ICaLCa + ICaLK+ICaLNa;
      else
          ICaLNa =
(0.00005*PCAL*CfNa)*mcal*hcal;
          ICaLK = (0.001 * PCAL * CfK)*mcal*hcal;
          ICaLCa = (PCAL * CfCa*mcal*hcal);
          ICaL = ICaLCa + ICaLK+ICaLNa;
          [mcal, hcal] =
calcRateConst(1,Va,0,Cai,mcal,hcal,count,dt); %Calc
m and h
      end
  
```

# The Underlying Problem?

## The Publishing Process

model creation



translated into text and equations for publication

which cotransporters are to be included in the model. Note that eqs. (3) imply that the total number of  $\text{Cl}^-$  and  $\text{HCO}_3^-$  ions and the sum of the number of  $\text{K}^+$  and  $\text{Na}^+$  ions in the ECS and the astrocyte are conserved at any time. Ion flux through  $\text{KCC1}$ ,  $\text{NKCC1}$ <sup>(52)</sup> and  $\text{NBC}$ <sup>(45,53)</sup> is modeled in a Nernst-like fashion, i.e.

$$(5) J_{\text{KCC1}} = \frac{g_{\text{KCC1}}}{F} \frac{RT}{F} \ln \left( \frac{[\text{K}^+]_o [\text{Cl}^-]_o}{[\text{K}^+]_i [\text{Cl}^-]_i} \right),$$

$$(6) J_{\text{NBC}} = \frac{g_{\text{NBC}}}{F} [V_m - E_{\text{NBC}}],$$

$$(7) J_{\text{NKCC1}} = \frac{g_{\text{NKCC1}}}{F} \frac{RT}{F} \ln \left( \frac{[\text{Na}^+]_o [\text{K}^+]_o ([\text{Cl}^-]_o)^2}{[\text{Na}^+]_i [\text{K}^+]_i ([\text{Cl}^-]_i)^2} \right).$$

Here,  $g_{\text{NKCC1}}$ ,  $g_{\text{KCC1}}$  and  $g_{\text{NBC}}$  are the conductances per unit area for the  $\text{NKCC1}$ , the  $\text{KCC1}$  and  $\text{NBC}$  cotransporter, respectively. The reversal potential of  $\text{NBC}$  is

$$(8) E_{\text{NBC}} = \frac{RT}{z_{\text{NBC}} F} \ln \left( \frac{[\text{Na}^+]_o [\text{HCO}_3^-]_o^2}{[\text{Na}^+]_i [\text{HCO}_3^-]_i^2} \right),$$

where  $z_{\text{NBC}}$  is the effective valence of the  $\text{NBC}$  cotransporter complex, here taken to be  $-1$ , setting  $z_{\text{NBC}} = -(n - 1) = -1$  where  $n$  is the stoichiometry, and adopting  $n = 2$ .

The assumed electroneutrality condition demands that the algebraic sum of all electric currents into the astrocyte has to be zero at every instant. The astrocytic membrane potential  $V_m$  is then given by solving the resulting equation with respect to  $V_m$ ;

$$(9) V_m = \frac{g_{\text{Na}} E_{\text{Na}} + g_{\text{K}} E_{\text{K}} + g_{\text{Cl}} E_{\text{Cl}} + \theta_{\text{NBC}} g_{\text{NBC}} E_{\text{NBC}} - J_{\text{NaKATPase}} F}{g_{\text{Na}} + g_{\text{K}} + g_{\text{Cl}} + \theta_{\text{NBC}} g_{\text{NBC}}}.$$

The rate of change of the astrocytic volume relative to its surface area,  $\frac{\dot{V}_i}{V_i} = v_i/A$ , is, by

# The Underlying Problem?

## The Publishing Process

model creation



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reviewed & published

The cell membrane is modeled as a capacitor connected in parallel with variable resistances and batteries representing the different ionic currents and pumps. The electrophysiological behavior of a single cell can hence be described with the following differential equation (23)

$$\frac{dV}{dt} = -\frac{I_{ion} + I_{stim}}{C_m} \quad (1)$$

where  $V$  is voltage,  $t$  is time,  $I_{ion}$  is the sum of all transmembrane ionic currents,  $I_{stim}$  is the externally applied stimulus current, and  $C_m$  is cell capacitance per unit surface area.

Similarly, ignoring the discrete character of microscopic cardiac cell structure, a 2D sheet of cardiac cells can be modeled as a continuous system with the following partial differential equation (23)

$$\frac{\partial V}{\partial t} = -\frac{I_{ion} + I_{stim}}{C_m} + \frac{1}{\rho_x S_x C_m} \frac{\partial^2 V}{\partial x^2} + \frac{1}{\rho_y S_y C_m} \frac{\partial^2 V}{\partial y^2} \quad (2)$$

where  $\rho_x$  and  $\rho_y$  are the cellular resistivity in the  $x$  and  $y$  directions,  $S_x$  and  $S_y$  are the surface-to-volume ratio in the  $x$  and  $y$  directions, and  $I_{ion}$  is the sum of all transmembrane ionic currents given by the following equation

$$I_{ion} = I_{Na} + I_{K1} + I_{Ca} + I_{Kr} + I_{Ks} + I_{CaL} + I_{NaCa} + I_{NaK} \\ + I_{pCa} + I_{pK} + I_{CaB} + I_{Kb} \quad (3)$$

where  $I_{NaCa}$  is  $\text{Na}^+/\text{Ca}^{2+}$  exchanger current,  $I_{NaK}$  is  $\text{Na}^+/\text{K}^+$  pump current,  $I_{pCa}$  and  $I_{pK}$  are plateau  $\text{Ca}^{2+}$  and  $\text{K}^+$  currents, and  $I_{CaB}$  and  $I_{Kb}$  are background  $\text{Ca}^{2+}$  and  $\text{K}^+$  currents.

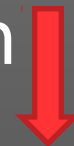
# The Underlying Problem?

## The Publishing Process

model creation



translated into text and  
equations for  
publication



reviewed & published



interpreted & implemented

```

%-----Calc the L-type Ca
current-----

      [CfCa,RevPCa]=
CalcConstantfield(Cai,Cao,2, Vm); %Ca
      [CfK,RevPK] =
CalcConstantfield(Ki,Ko,1, Vm); %K
      [CfNa,RevPNa] =
CalcConstantfield(Nai,Nao,1, Vm); %Na
      if (count ==1 && currenttime == 0)
          Va = -74.0078;
      else
          Va = Vm;
      end
      if (count ==0)
          [mcal, hcal,n] =
calcRateConst(1,Va,0,Cai,mcal,hcal,count,dt);
%Calc m and h
          ICaLNa =
(0.00005*PCAL*CfNa)*mcal*hcal;
          ICaLK = (0.001 * PCAL *
CfK)*mcal*hcal;
          %ICaLNa = (PCAL * CfCa*mcal*hcal);
%original
          ICaLNa = (PCAL * CfCa*mcal*hcal);
          ICaL = ICaLNa + ICaLK+ICaLNa;
      else
          ICaLNa =
(0.00005*PCAL*CfNa)*mcal*hcal;
          ICaLK = (0.001 * PCAL *
CfK)*mcal*hcal;
          ICaLNa = (PCAL * CfCa*mcal*hcal);
          ICaL = ICaLNa + ICaLK+ICaLNa;
          [mcal, hcal] =
calcRateConst(1,Va,0,Cai,mcal,hcal,count,dt);
%Calc m and h
    
```



# The Underlying Problem?

## The Publishing Process

```

%-----Calc the L-type Ca
current-----

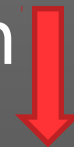
      [CfCa,RevPCa]=
CalcConstantfield(Cai,Cao,2, Vm); %Ca
      [CfK,RevPK] =
CalcConstantfield(Ki,Ko,1, Vm); %K
      [CfNa,RevPNa] =
CalcConstantfield(Nai,Nao,1, Vm); %Na
      if (count ==1 && currenttime == 0)
          Va = -74.0078;
      else
          Va = Vm;
      end
      if (count ==0)
          [mcal, hcal,n] =
calcRateConst(1,Va,0,Cai,mcal,hcal,count,dt);
%Calc m and h
          ICaLNa =
(0.00005*PCAL*CfNa)*mcal*hcal;
          ICaLK = (0.001 * PCAL *
CfK)*mcal*hcal;
          %ICaLNa = (PCAL * CfCa*mcal*hcal);
%original
          ICaLNa = (PCAL * CfCa*mcal*hcal);
          ICaL = ICaLNa + ICaLK+ICaLNa;
      else
          ICaLNa =
(0.00005*PCAL*CfNa)*mcal*hcal;
          ICaLK = (0.001 * PCAL *
CfK)*mcal*hcal;
          ICaLNa = (PCAL * CfCa*mcal*hcal);
          ICaL = ICaLNa + ICaLK+ICaLNa;
          [mcal, hcal] =
calcRateConst(1,Va,0,Cai,mcal,hcal,count,dt);
%Calc m and h
    
```

model creation



error

translated into text and  
equations for  
publication



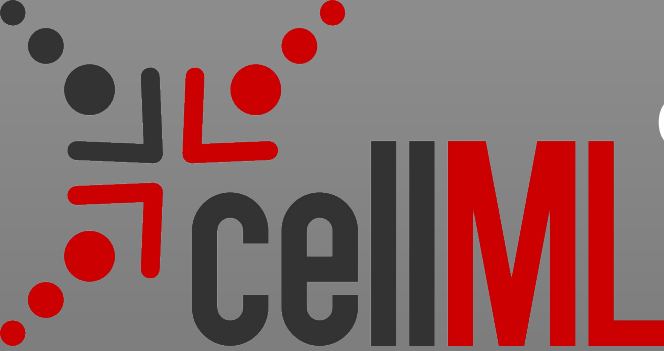
error

reviewed & published



error

interpreted & implemented



# CellML has been developed as a potential solution to the inconsistencies between computational and published models

```

<component name="membrane">
  <variable units="millivolt" public_interface="out" name="V" initial_value="86.2" />
  <variable units="microF" public_interface="out" name="Cm" initial_value="0.185" />
  <variable units="micrometre3" public_interface="out" name="V_c" initial_value="0.016404" />
  <variable units="millisecond" public_interface="in" name="time" />
  <variable units="picoA_per_picoF" public_interface="in" name="i_K1" />
  <variable units="picoA_per_picoF" public_interface="in" name="i_Ks" />
  <variable units="picoA_per_picoF" public_interface="in" name="i_CaL" />
  <variable units="picoA_per_picoF" public_interface="in" name="i_NaK" />
  <variable units="picoA_per_picoF" public_interface="in" name="i_p_K" />

  <math xmlns="http://www.w3.org/1998/Math/MathML">
    <apply><eq />
      <apply><diff />
        <bvar><ci>time</ci></bvar>
        <ci>V</ci>
      </apply>
      <times />
      <apply><divide />
        <apply><minus />
          <cn cellml:units="dimensionless">1</cn>
        </apply>
        <cn cellml:units="dimensionless">1</cn>
      </apply>
      <plus /><ci>i_K1</ci>
      <ci>i_to</ci><ci>i_Kr</ci>
      <ci>i_b_Na</ci><ci>i_NaCa</ci>
      <ci>i_b_Ca</ci><ci>i_p_K</ci>
      <ci>i_p_Ca</ci><ci>i_Stim</ci>
    </apply>
  </math>
</component>

```

The cell membrane is modeled as a capacitor connected in parallel with variable resistances and batteries representing the different ionic currents and pumps. The electrophysiological behavior of a single cell can hence be described with the following differential equation (23)

$$\frac{dV}{dt} = -\frac{I_{ion} + I_{stim}}{C_m} \quad (1)$$

where  $V$  is voltage,  $t$  is time,  $I_{ion}$  is the sum of all transmembrane ionic currents,  $I_{stim}$  is the externally applied stimulus current, and  $C_m$  is cell capacitance per unit surface area.

Similarly, ignoring the discrete character of microscopic cardiac cell structure, a 2D sheet of cardiac cells can be modeled as a continuous system with the following partial differential equation (23)

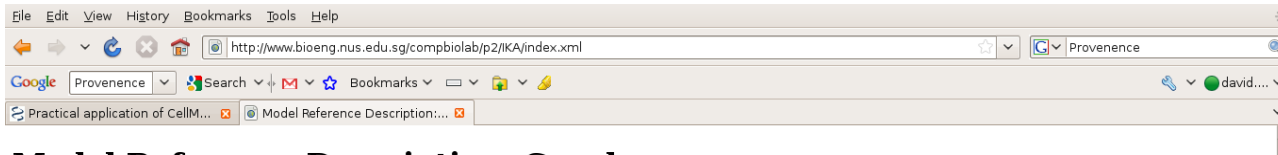
$$\frac{\partial V}{\partial t} = -\frac{I_{ion} + I_{stim}}{C_m} + \frac{1}{\rho_x S_x C_m} \frac{\partial^2 V}{\partial x^2} + \frac{1}{\rho_y S_y C_m} \frac{\partial^2 V}{\partial y^2} \quad (2)$$

where  $\rho_x$  and  $\rho_y$  are the cellular resistivity in the  $x$  and  $y$  directions,  $S_x$  and  $S_y$  are the surface-to-volume ratio in the  $x$  and  $y$  directions, and  $I_{ion}$  is the sum of all transmembrane ionic currents given by the following equation

$$I_{ion} = I_{Na} + I_{K1} + I_{to} + I_{Kr} + I_{Ks} + I_{CaL} + I_{NaCa} + I_{NaK} + I_{pCa} + I_{pK} + I_{bCa} + I_{bNa} \quad (3)$$

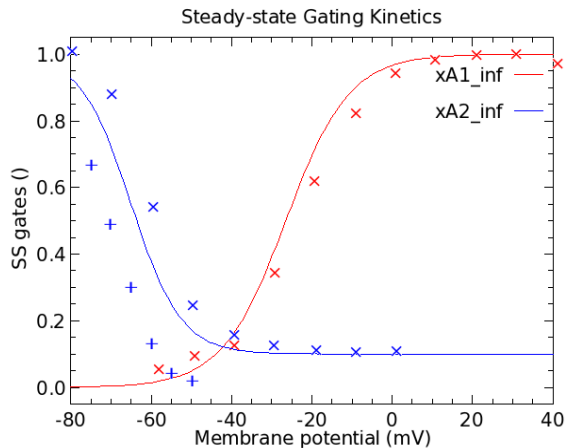
where  $I_{NaCa}$  is  $Na^+/Ca^{2+}$  exchanger current,  $I_{NaK}$  is  $Na^+/K^+$  pump current,  $I_{pCa}$  and  $I_{pK}$  are plateau  $Ca^{2+}$  and  $K^+$  currents, and  $I_{bCa}$  and  $I_{bK}$  are background  $Ca^{2+}$  and  $K^+$  currents.

# Reproduction and provenance



## Model Reference Description: Graphs

Steady-state Gating Kinetics  
Creator: David Nickerson (david.nickerson@nus.edu.sg) Division of Bioengineering, National University of Singapore  
Created: 2007-11-27  
Publisher: Division of Bioengineering, National University of Singapore



**xA1\_inf**  
x-axis  
Simulation: ...A-voltage-clamp.xml#simulation  
Variable: ...ments/IKA-voltage-clamp.xml#Vm  
y-axis  
Simulation: ...A-voltage-clamp.xml#simulation  
Variable: ...ist/components/IKA.xml#xA1\_inf  
Experimental Data  
x

IKA steady state activation gating kinetics  
Amberg et al (2002).  
Creator: David Nickerson (david.nickerson@nus.edu.sg) Division of Bioengineering, National University of Singapore  
Created: 2007-11-24  
Pubmed reference: [12381815](https://pubmed.ncbi.nlm.nih.gov/12381815/)  
Biological Entity: gastric antrum  
Species: mouse  
Data source: ...ate-gating-data-activation-header=present]  
Comment:  
Data used to fit the steady state activation kinetics of the IKA current in the (2007) smooth muscle cellular electrophysiology model.  
Modification [modified by David Nickerson]  
Splitting the combined data into series for ease of use.  
Modified: 2007-11-26

**xA2\_inf**

BIOINFORMATICS APPLICATIONS NOTE Vol. 24 no. 8 2008, pages 1112–1114 doi:10.1093/bioinformatics/btn080

Systems biology

## Reference descriptions of cellular electrophysiology models

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Division of Bioengineering, National University of Singapore, Singapore

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Associate Editor: Olga Troyanskaya

### ABSTRACT

**Summary:** In recent years there has been much development of the fundamental ideas underlying mathematical model curation in regard to models of biology. While much has been achieved in the realms of systems biology and bioinformatics, little progress has been made in relation to cellular electrophysiology modeling. The primary reason for slow progress in this field is the lack of a consistent and machine-readable reference description for a given model. CellML has been widely used to describe mathematical models of cellular electrophysiology in an unambiguous, machine-readable format. Through the use of well-annotated CellML models we propose a standard by which reference descriptions of cellular electrophysiology models can be similarly defined in an unambiguous, software independent, and machine-readable format. Adoption of this standard will provide a consistent technology by which cellular electrophysiology models can be curated.

**Availability:** <http://www.bioeng.nus.edu.sg/compbiolab/p2/>

**Contact:** david.nickerson@nus.edu.sg

**Supplementary information:** Example reference descriptions are available at <http://www.bioeng.nus.edu.sg/compbiolab/p2/>

### 1 INTRODUCTION

There is a long history of publication of mathematical models of cellular electrophysiology, dating back to the seminal work of Hodgkin and Huxley (1952). Historically, cellular electrophysiology model developments and justifications are well specified in the model's original journal publication whereas the mathematical model itself is not always specified in such great detail. Additionally, complete parametrization and specification of required boundary conditions for particular numerical simulations using the models are not always present—often due to requirements to provide a concise description of the model in traditional journal publication formats. Furthermore, the actual numerical and computational methods used to perform simulations are generally even less well defined in the original model publication. These factors make it very difficult for

As an aid to overcome these shortcomings, model authors often use the Internet to distribute computer code for their own implementation of their model(s). A good example of this is the Rudy lab (<http://rudylab.wustl.edu/>), which provides source code for the widely used LRD-based model series. While useful as an aid to enable scientists to utilize mathematical models, there is usually no direct relationship between a model's publication and any provided code. As such, there is still no easy way to check a new implementation of the model or quantitatively compare the model's implementation with results from the model's original publication. An example of this is when such models must be re-implemented in a specific format for inclusion in other tools, such as the use of LRD models in whole heart electrophysiology modeling.

In the field of systems biology, much effort has been invested in creating validated and curated models, such that models can be reused and combined in new ways (see, for example, <http://www.biomodels.net/>). The MIRIAM standard (Le Novère *et al.*, 2005) has been established to guide such curation and is equally applicable to whole-cell electrophysiology models but has not yet been widely applied in this area. In order to be able to curate an implementation of an electrophysiology model it is essential to have an authoritative version of the model against which the implementation can be critically evaluated. In the MIRIAM standard this is referred to as the model's *reference description* and here we put forward a standard suitable for defining reference descriptions of cellular electrophysiology models.

### 2 APPROACH

CellML (<http://www.cellml.org>) has previously been shown as a versatile tool for the definition (Nickerson and Hunter, 2006) and utilization (Nickerson *et al.*, 2006) of cellular electrophysiology models. As such, we use CellML for the base definition of the mathematical model and use CellML related technology in the definition of a reference description. The same technology could, however, be applied equally well to mathematical models specified in other standard formats.

<http://www.bioeng.nus.edu.sg/compbiolab/p2/>

doi:10.1093/bioinformatics/btn080

Reference Description of a HH-based Modelling Study  
David Nickerson (2008-07-16)

Reference Description of a HH-based Modelling Study  
David Nickerson et al (2021)

David Nickerson, D P Nickerson & Andre. 'Investigation of membrane conductance and ion concentrations using Hodgkin & Huxley's squid axon model'. *Fan J Eve Cool*. 2021 Jun;1(1):12-67

Last modified: 2008-09-14, D P Nickerson (Created: 2008-07-16, David Nickerson)

Created: Wed 16 Jul 2008 12:00:00 AM MALST  
Creator: David Nickerson (david.nickerson@nus.edu.sg), Division of Bioengineering, National University of Singapore

| Date                              | Modification                                                                                                                                              | Modifier                                                                               |
|-----------------------------------|-----------------------------------------------------------------------------------------------------------------------------------------------------------|----------------------------------------------------------------------------------------|
| Thu 14 Aug 2008 12:00:00 AM MALST | Adding in the membrane conductance study.                                                                                                                 | D P Nickerson (biendp@nus.edu.sg)                                                      |
| Thu 14 Aug 2008 12:00:00 AM MALST | Adding in the ion concentration study.                                                                                                                    | Andre (david.nickerson@nus.edu.sg) of Bioengineering, National University of Singapore |
| Thu 31 Jul 2008 12:00:00 AM MALST | Adding in the potassium channel validation study.                                                                                                         | David Nickerson (david.nickerson@nus.edu.sg) of Bioengineering, National U Singapore   |
| Wed 23 Jul 2008 12:00:00 AM MALST | Re-wording some bits and pieces in order to add apostrophes (') to the text in order to test the escaping when generating the JSON reference description. | David Nickerson (david.nickerson@nus.edu.sg) of Bioengineering, National U Singapore   |
| Wed 16 Jul 2008 12:00:00 AM MALST | Escaped the HTML code in the description in order to get this RDF code to validate.                                                                       | David Nickerson (david.nickerson@nus.edu.sg) of Bioengineering, National U Singapore   |

This is a complete description of the models and numerical experiments performed in this Hodgkin Huxley based modelling article. Herein you will find all the information required to completely recreate and validate the work presented in the article.

This is a demonstration of the complete specification of a reference description of an entire cellular electrophysiology model publication. In this reference description you will find descriptions and results of simulation performed to validate the base model upon which this fictitious modelling article, as well as some fanciful modifications of the base model along with the novel insights obtained therefrom.

The reference description can be browsed via the tree hierarchy over on the left hand side of the page or from the list of tasks given below. All you need to do is assume that there is an associated, peer-reviewed article which summarises this reference description and perhaps provides some further analysis of the model mentioned above :)

Tasks:

- Model Validation
- The effect of membrane conductance
- Varying ion concentrations

Generated by: CellMLSimulator (version: CellMLSimulator 0.3.0-devel-json - revision 132M - Thu Aug 14 18:14:54 SGT 2008) at Fri 15 Aug 2008 11:56:42 AM MALST

30th Annual International IEEE EMBS Conference  
Vancouver, British Columbia, Canada, August 20-24, 2008

## Interactive reference descriptions of cellular electrophysiology models

David Nickerson and Martin Buist

**Abstract**—With the advent and popularization of technologies such as CellML and SBML, it has become relatively easy to share and exchange mathematical models of biological systems. However, as such technology evolves it is inevitable that not all tools will correctly interpret the full range of models able to be described. It is also necessary to completely describe the mathematical models allowing model users to appropriately use each model. To address these issues we have previously developed methods and tools based on community defined standards which allow for the specification of a reference description of a mathematical model. Such reference descriptions provide a comprehensive description of both the mathematical model and the outcomes expected when performing specific numerical simulations using the model. Thus providing for quantitative validation of tool interpretation of a given model as well as informing the model user as to all aspects of the model definition. Further development of this work has led to the conclusion that presenting such reference descriptions in a user friendly and interactive manner provides a powerful tool for the dissemination and understanding of the mathematical model. Furthermore, such a tool is seen as an invaluable teaching aid in the education of biomedical engineers and scientists allowing for anything from a superficial to a very comprehensive interaction with the mathematical model.

### I. INTRODUCTION

With the aid of current technology, it is now easier than ever for mathematical model developers to share their models with collaborators and the scientific community. The use of CellML [1, <http://www.cellml.org>] or SBML [2, <http://sbml.org>], for example, makes it possible to exchange mathematical model descriptions between many research groups using independent software tools. We are now seeing the evolution of freely available repositories of curated model descriptions (see, for example, <http://www.cellml.org/models/> and <http://www.biomodels.net> [3]) to provide important and useful archives of model descriptions. There remains, however, questions such as just what a particular mathematical model is describing? where do all the parameter values come from? what data was used to fit this relationship? and so on.

A large step toward addressing these questions was made with the specification of the MIRIAM<sup>1</sup> standard [4]. In part, the MIRIAM standard is based upon the idea of having a reference description of a mathematical model, which can then be annotated with relevant information in order to provide a complete description of the model. Previously,

we have presented a method whereby community standards being developed as part of the CellML project can be used to define comprehensive reference descriptions of mathematical models [5]. The outcome of this earlier work provides a machine interpretable description of the mathematical model which includes everything from parameter value sources, to experimental data utilized in model fitting and validation, to the actual graphical outputs included in the peer reviewed publication of the model. We have shown how a static rendering of this model description may be presented to human users in a manner which allows the description to be fully navigated by the user, with examples based on CellML and SBML available at <http://www.bioeng.nus.edu.sg/combiolab/p2>.

In addition to questions arising from the model itself, there is also the issue of whether all of the various tools supporting these technologies interpret the mathematical model in exactly the same manner (cf. the way in which web pages may look and/or behave differently in different web browsers). As these mathematical model description technologies evolve tool developers are inevitably forced to focus on the developments most relevant to their particular user requirements. Now that tools such as the CellML API (<http://www.cellml.org/tools/api>) and libSBML [6] are available, the hope is to standardize on such community defined tools for the core interpretation of the models while specific tool developers can build on top of that common foundation to meet their specific requirements. There are currently, however, sufficient independent tools in common usage that there can be no assurance that they all interpret the models in exactly the same manner.

As described above, the method we have presented previously [5] for the specification of comprehensive reference descriptions is a machine interpretable description of the mathematical model. As such, software tools are able to process the entire description and perform various tests upon it. Such tests may include checks on MIRIAM compliance, validity of the model encoding (e.g., SBML or CellML), consistency of physical units. In addition, the reference description includes data obtained from the numerical simulations used as part of the creation of the reference description (i.e., the data used to create the graphs included in the reference description) and links to experimental data used in the development of the actual mathematical model.

# Model exchange and reuse



# FAQ 1: why can't we just use MATLAB?

Not the only model description language

- Even where MATLAB is used – as a procedural language it is distinct from the published model
- A CellML model is a pure representation of the maths in the published paper

```
%-----Calc the L-type Ca
current-----

        [CfCa,RevPCa]=
CalcConstantfield(Cai,Cao,2, Vm); %Ca
        [CfK,RevPK] = CalcConstantfield(Ki,Ko,1,
Vm); %K
        [CfNa,RevPNa] =
CalcConstantfield(Nai,Nao,1, Vm); %Na
        if (count ==1 && currenttime == 0)
            Va = -74.0078;
        else
            Va = Vm;
        end
        if (count ==0)
            [mcal, hcal,n] =
calcRateConst(1,Va,0,Cai,mcal,hcal,count,dt);
%Calc m and h
            ICaLNa =
(0.00005*PCAL*CfNa)*mcal*hcal;
            ICaLK = (0.001 * PCAL * CfK)*mcal*hcal;
            %ICaLNa = (PCAL * CfCa*mcal*hcal);
%original
            ICaLNa = (PCAL * CfCa*mcal*hcal);
            ICaL = ICaLNa + ICaLK+ICaLNa;
        else
            ICaLNa =
(0.00005*PCAL*CfNa)*mcal*hcal;
            ICaLK = (0.001 * PCAL * CfK)*mcal*hcal;
            ICaLNa = (PCAL * CfCa*mcal*hcal);
            ICaL = ICaLNa + ICaLK+ICaLNa;
            [mcal, hcal] =
calcRateConst(1,Va,0,Cai,mcal,hcal,count,dt);
%Calc m and h
            :
```



## FAQ 2: this sounds a lot like SBML, why do both exist?

Historical reasons – both languages were started around 1999/2000 and were unaware the other existed

- Functional reasons – SBML and CellML have different emphases:
  - > “SBML is designed for representing models of biochemical reaction networks”. (<http://www.sbml.org/>)
  - > “The purpose of CellML is to store and exchange computer-based mathematical models”. (<http://www.cellml.org/>)



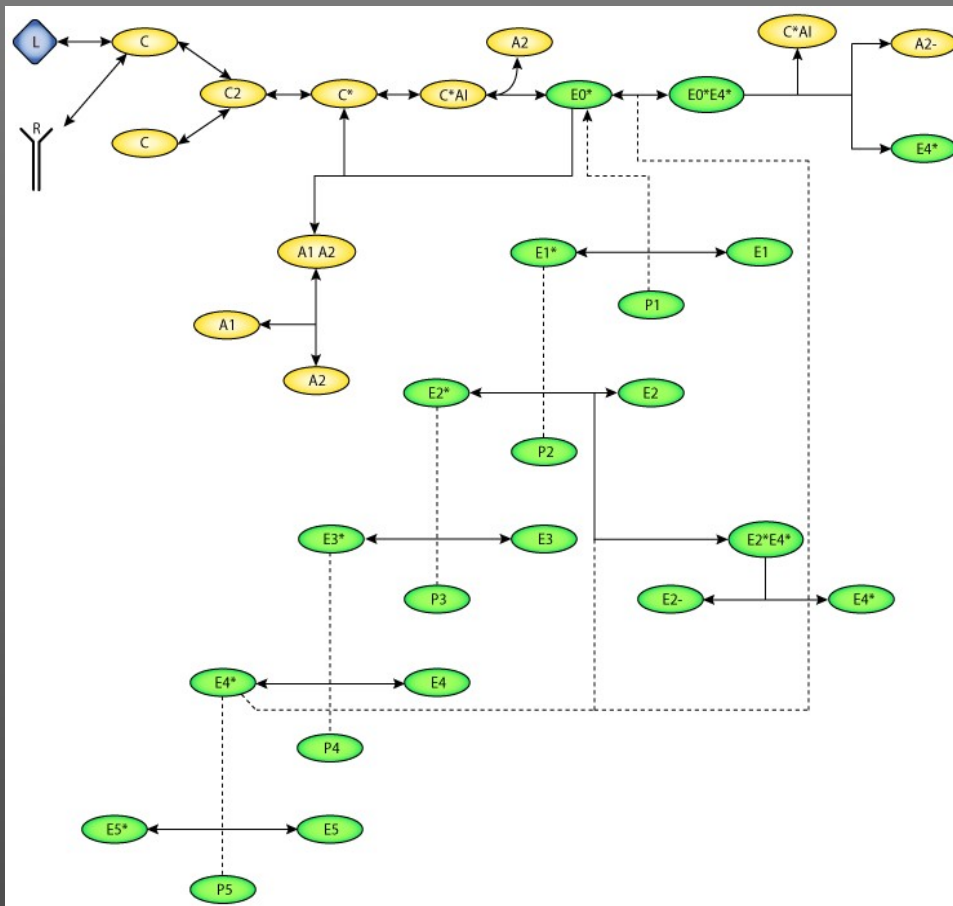


# CellML language features

CellML has a **flexible structure** and can be used to describe a diverse range of models... including...



CellML has a **flexible structure** and can be used to describe a diverse range of models... including...

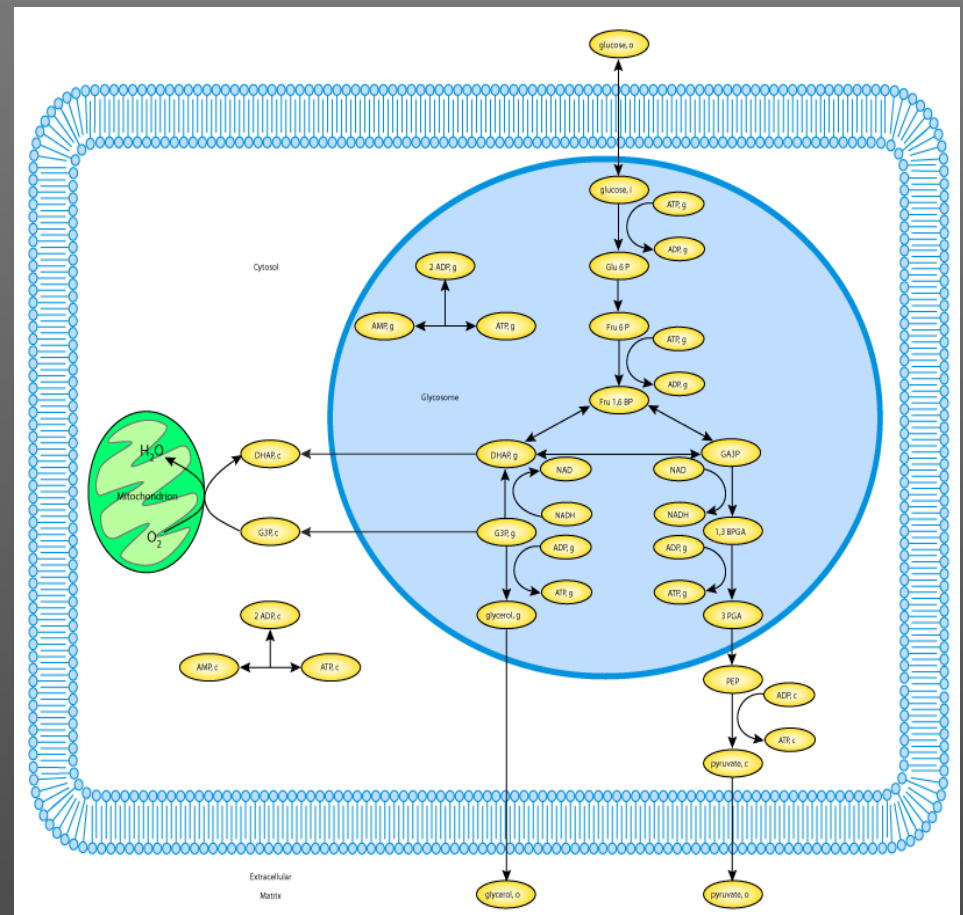


signal transduction

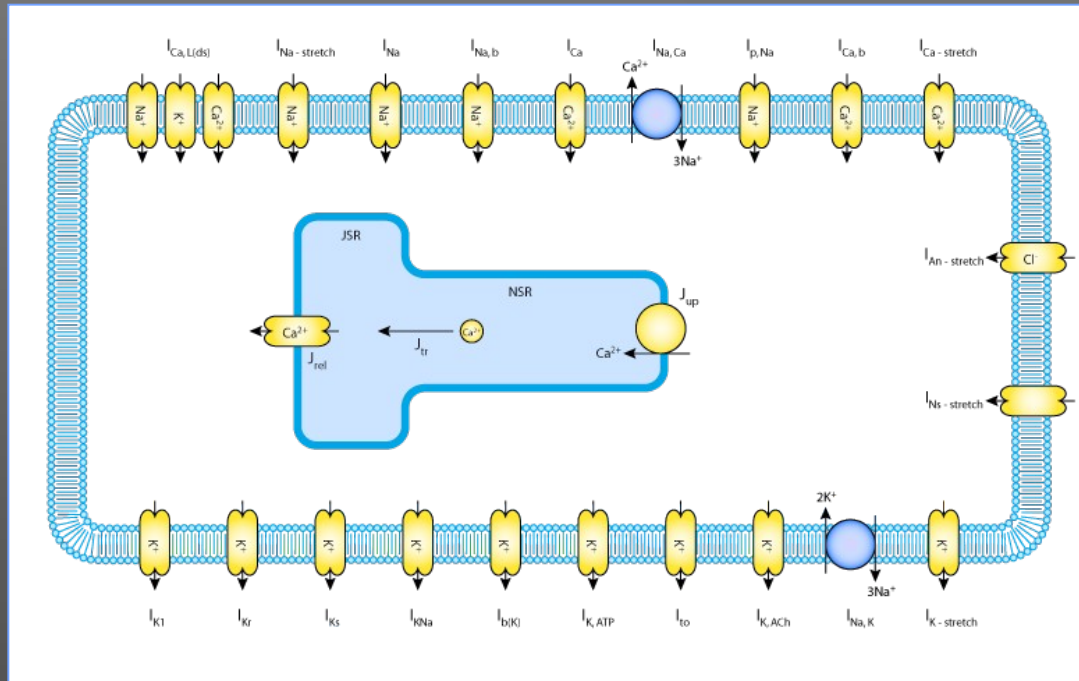
# CellML language features

CellML has a **flexible structure** and can be used to describe a diverse range of models... including...

metabolism



CellML has a **flexible structure** and can be used to describe a diverse range of models... including...

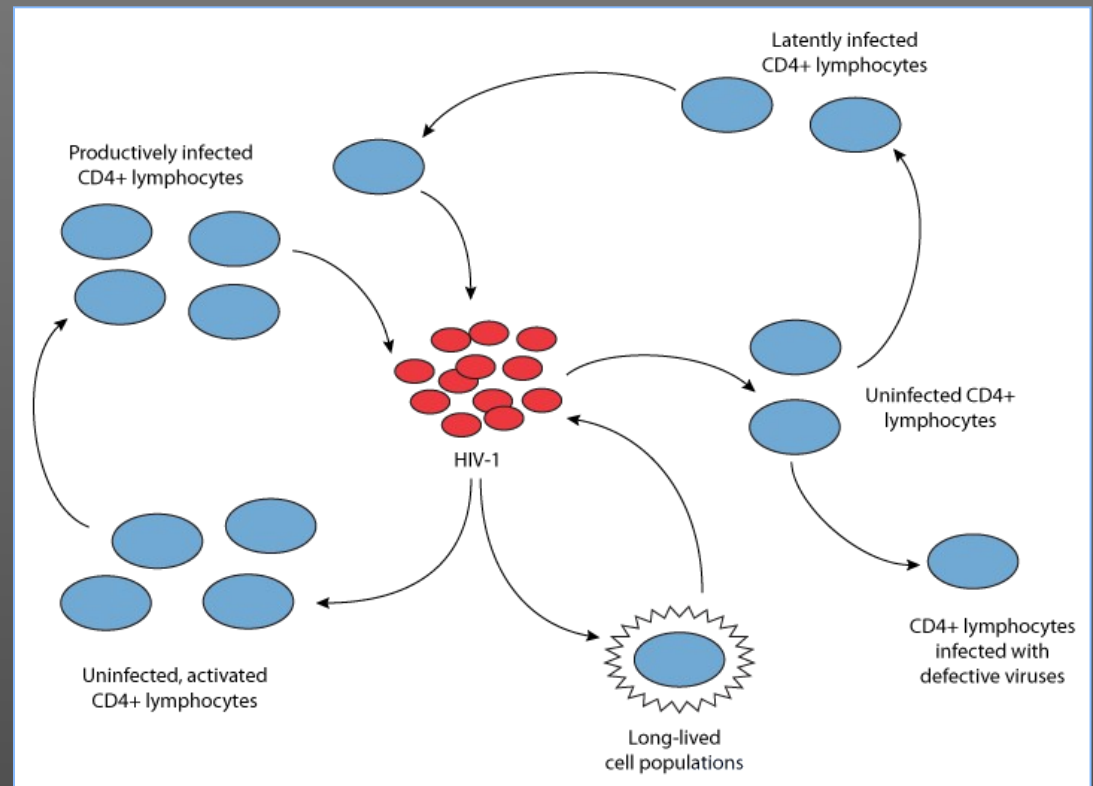


electrophysiology

# CellML language features

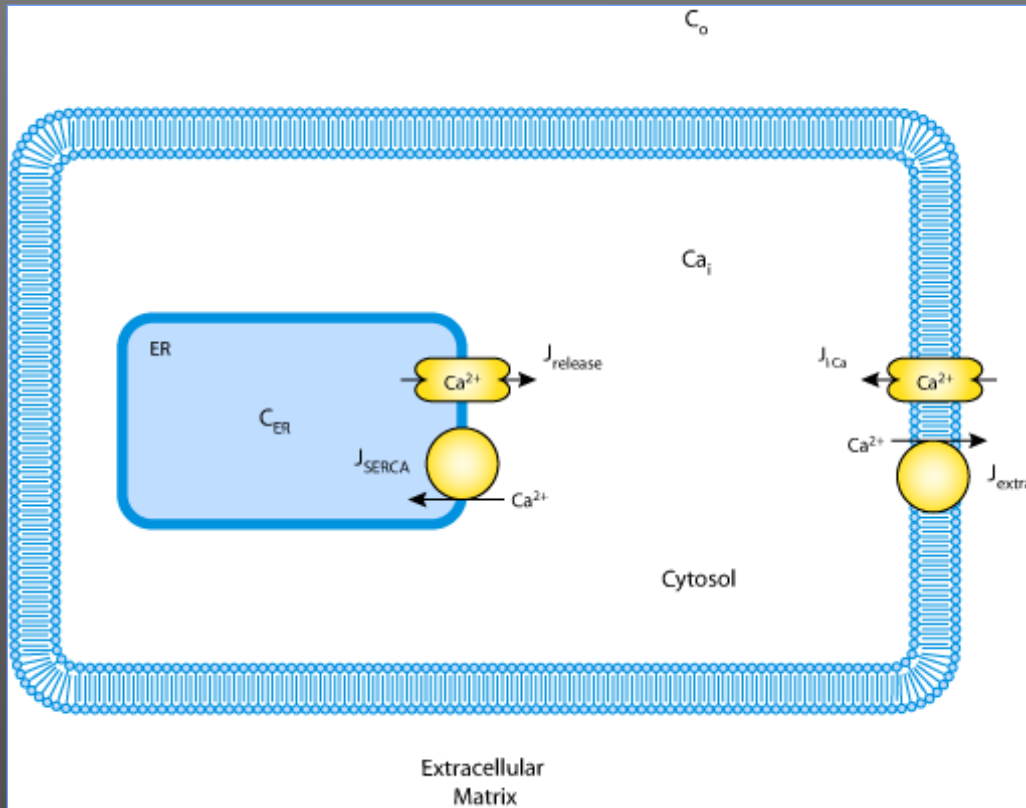
CellML has a **flexible structure** and can be used to describe a diverse range of models... including...

immunology



# CellML language features

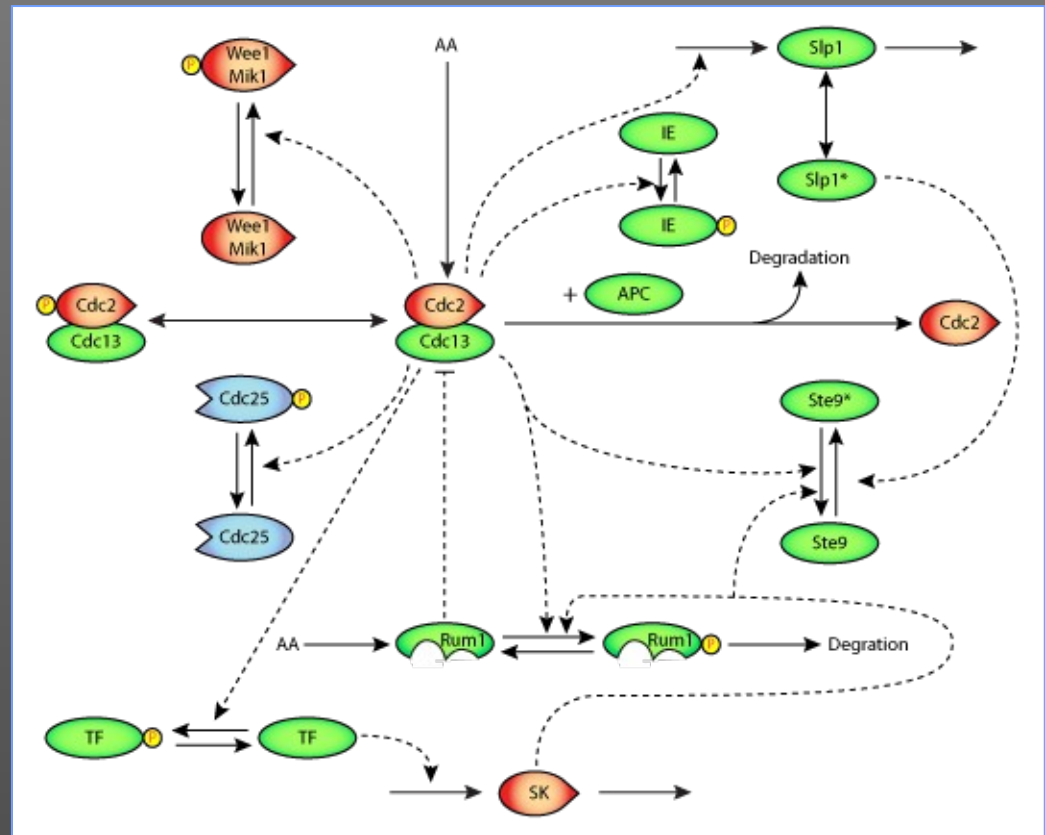
CellML has a **flexible structure** and can be used to describe a diverse range of models... including...



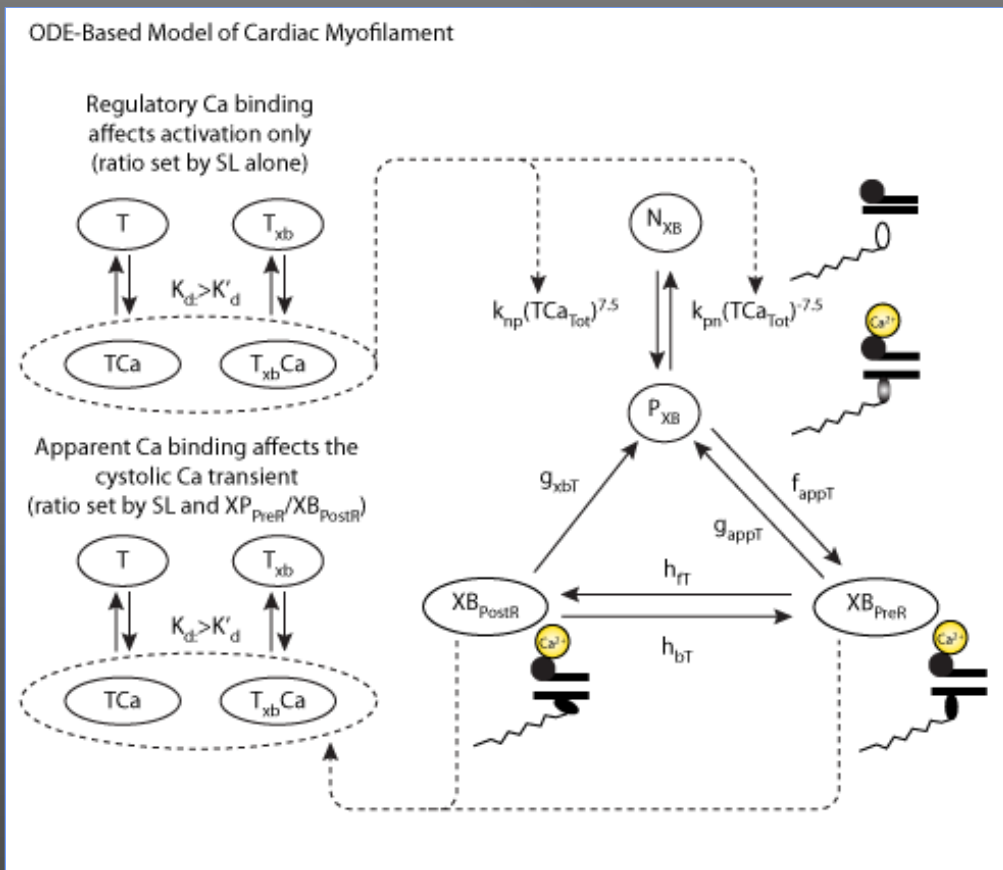
calcium dynamics

CellML has a **flexible structure** and can be used to describe a diverse range of models... including...

cell cycle



CellML has a **flexible structure** and can be used to describe a diverse range of models... including...

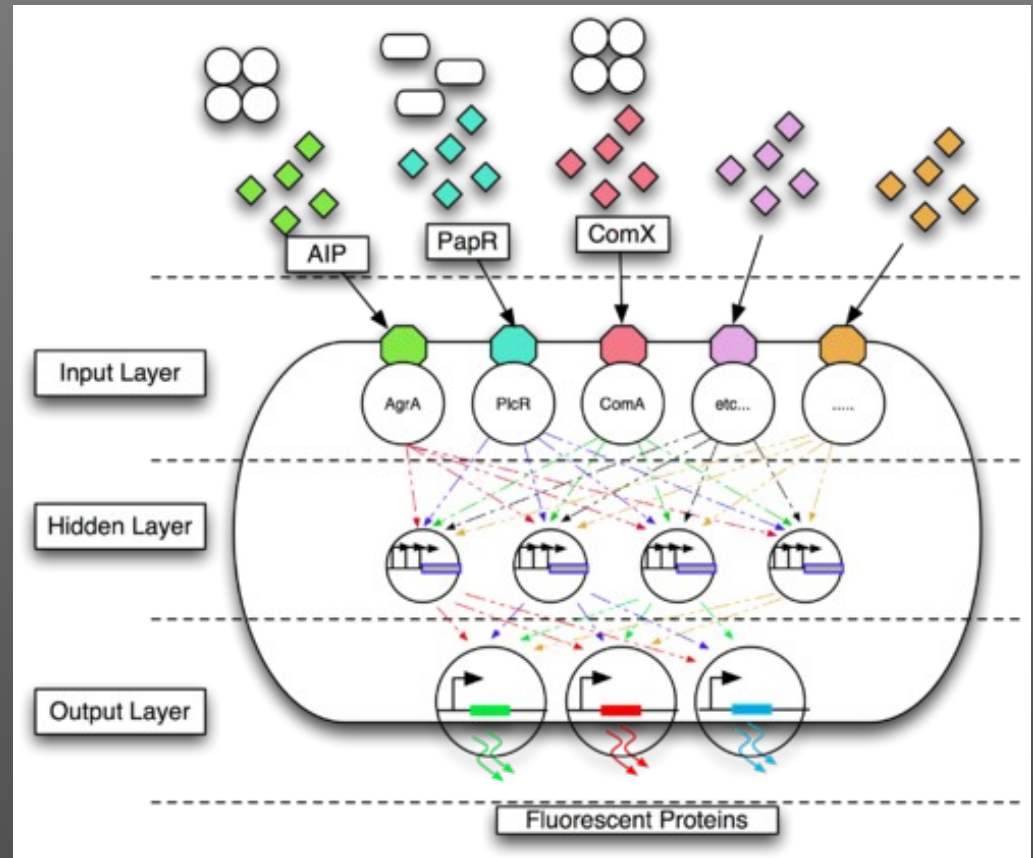


muscle contraction

# CellML language features

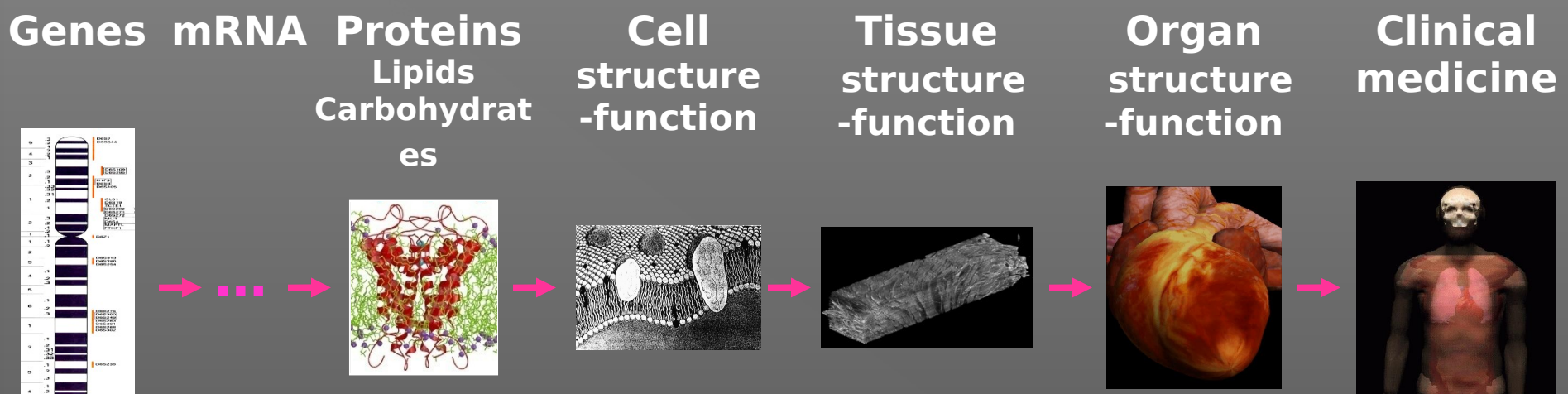
CellML has a **flexible structure** and can be used to describe a diverse range of models... including...

And synthetic biology





## A question of scale...



CellML



FieldML + OpenCMISS

CellML has 2 essential features which promote model exchange and reuse:

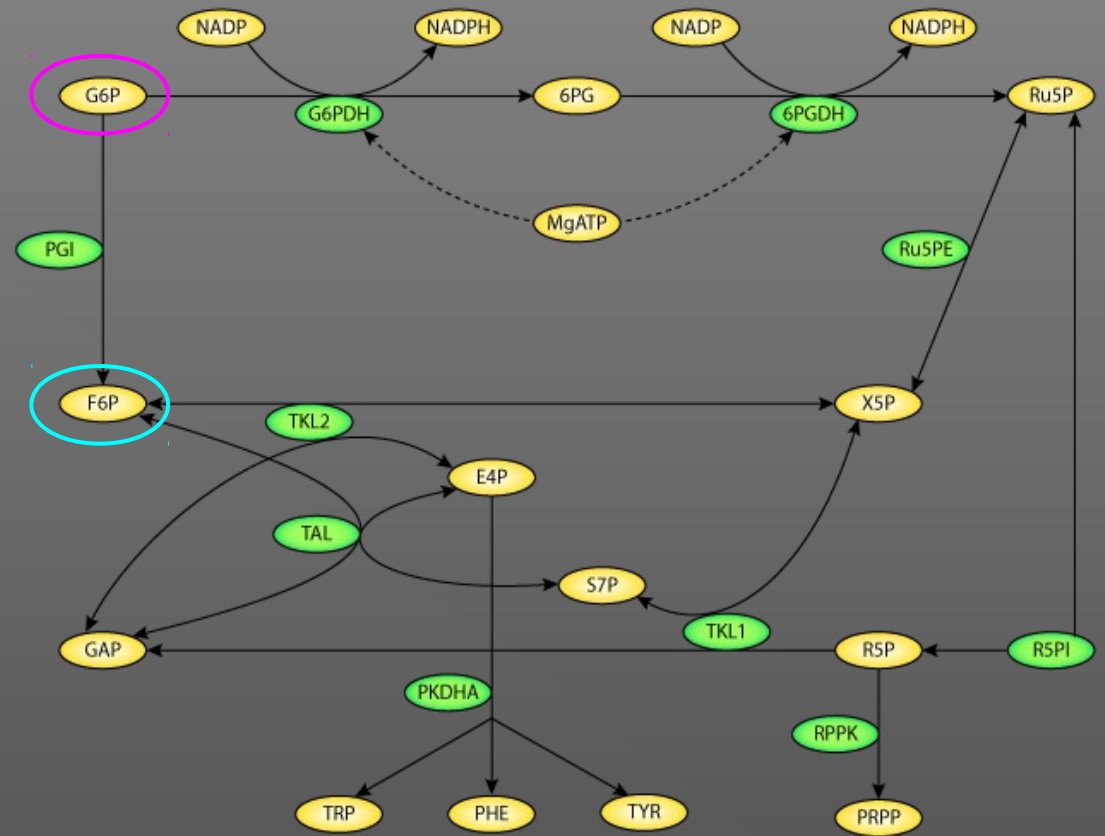
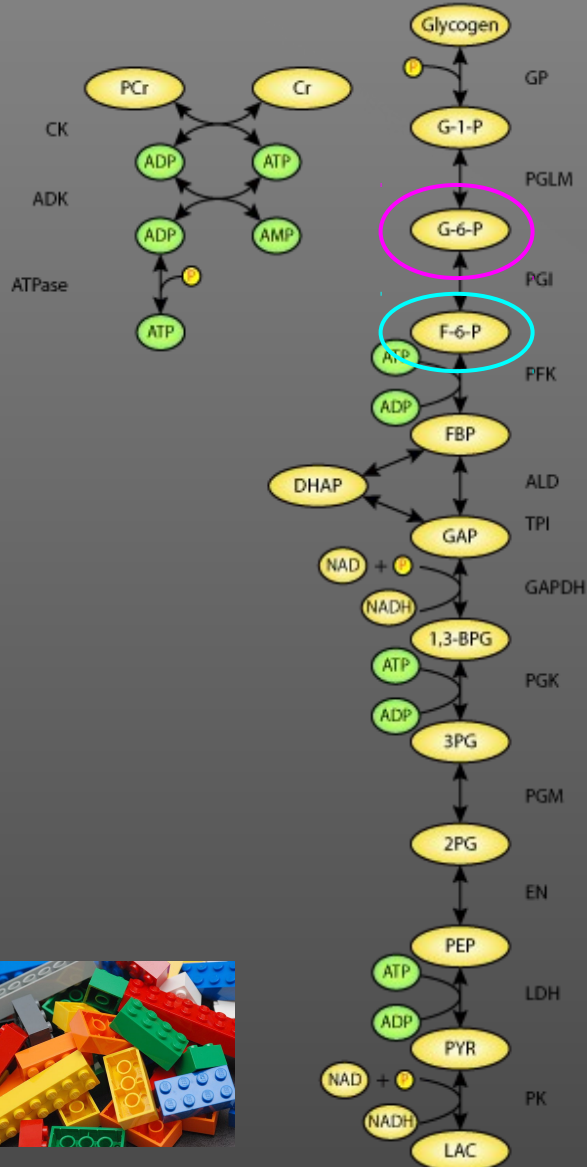
CellML has a **modular architecture**; allowing models to be broken down into “components”

- CellML 1.1 has an “**import**” feature which allows models to be connected and reused





# Model reuse 2: models can share entities & processes

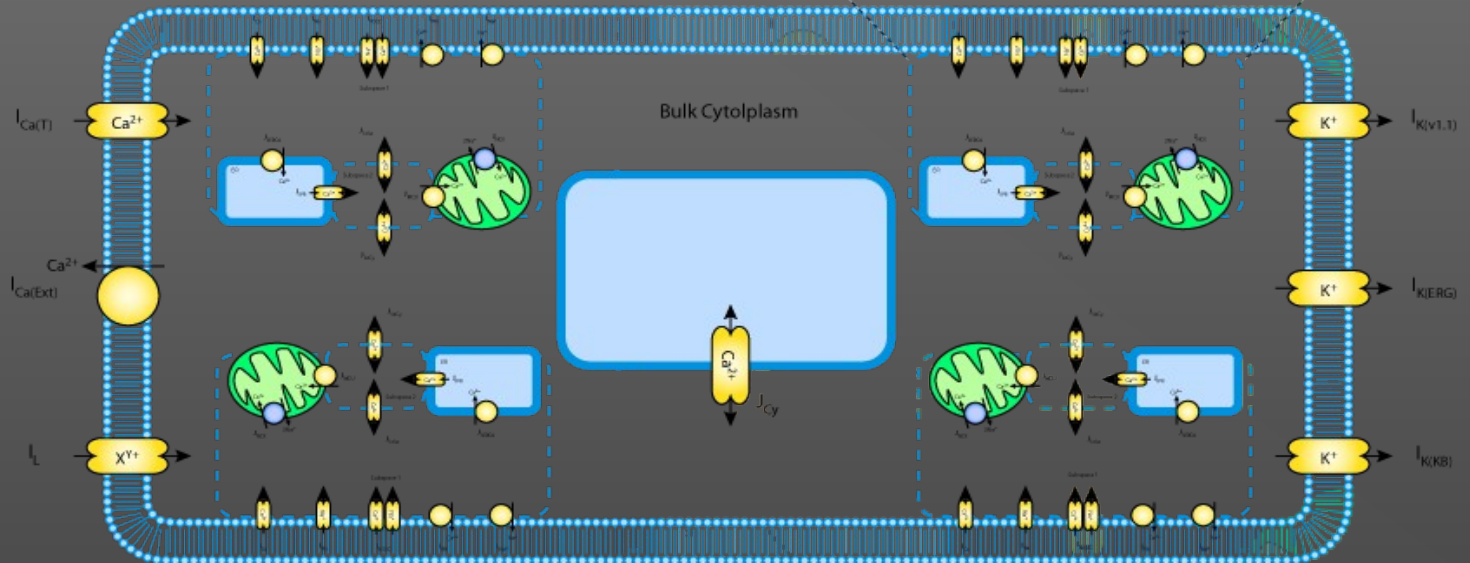
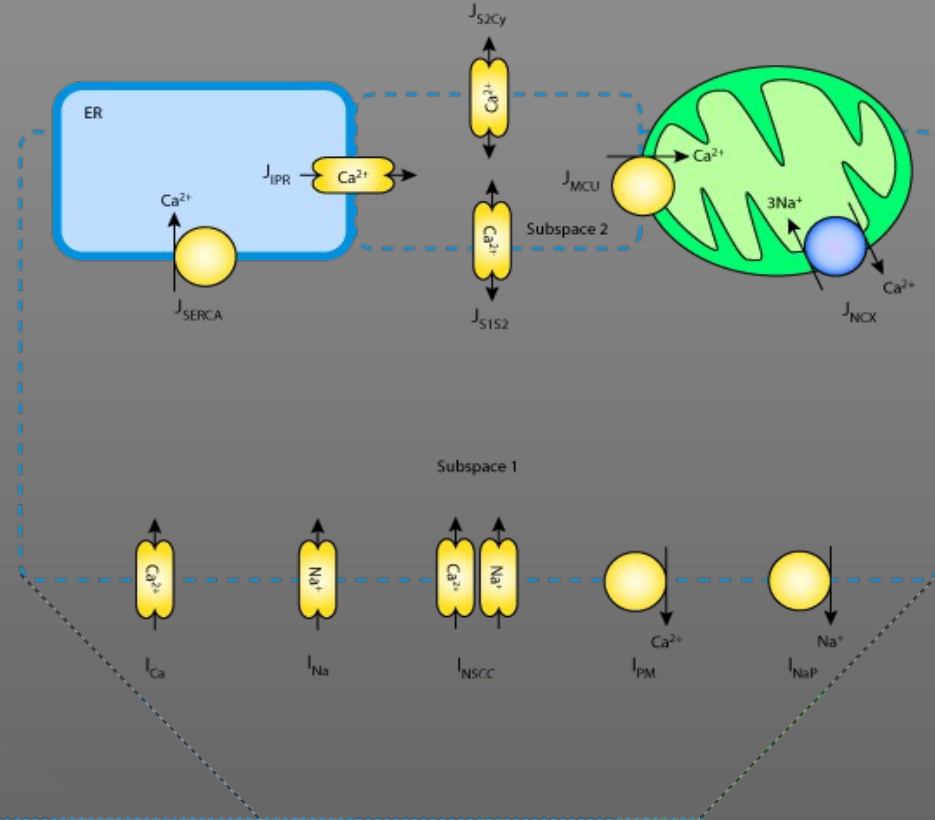


Some natural systems have a modular composition. Shared entities or processes can be reused between models.

# Model reuse 3: a model with a repeating unit

Faville *et al.* 2009

2 models: cell & pacemaker  
the pacemaker is defined once and is imported into the cell 10 times



# **CellML 1.1 modularity**

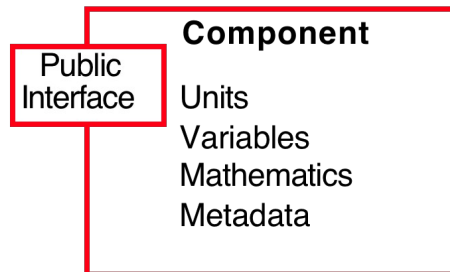
Poul Nielsen

# CellML

- CellML is designed to support the definition and sharing of models of biological processes.
- CellML includes information about:
  - Model structure (how the parts of a model are organizationally related to one another);
  - Mathematics (equations describing the underlying biological processes);
  - Metadata (additional information about the model that allows scientists to search for specific models or model components in a database or other repository).
- A public repository of over 500 published signal transduction, electrophysiological, mechanical, and metabolic pathway processes is available at *<http://models.cellml.org/>*

# CellML components

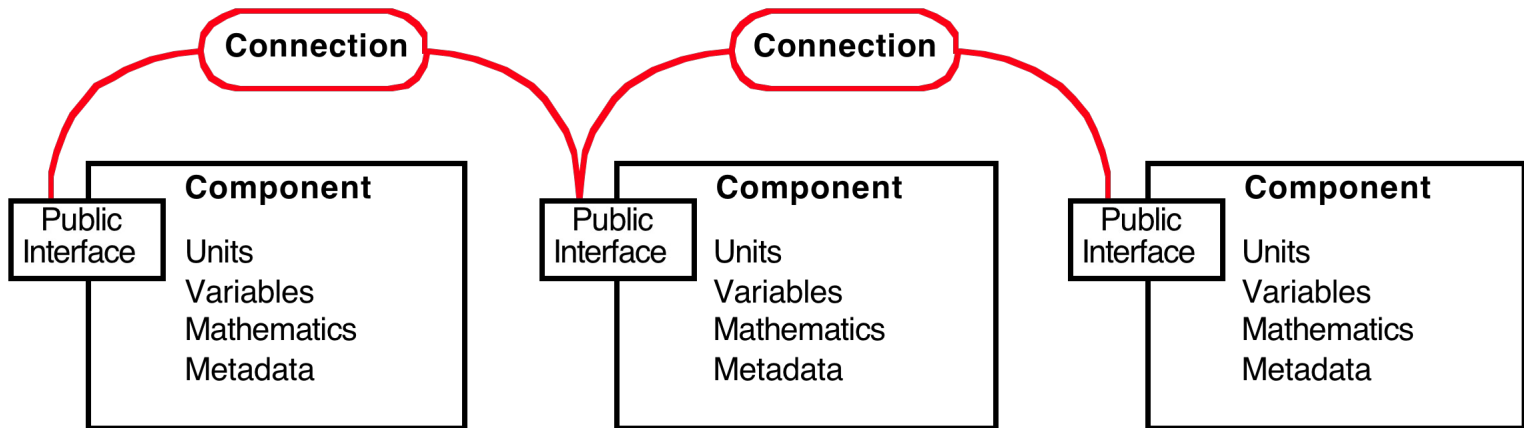
- CellML has a simple structure based upon connected *components*.
- Components abstract concepts by providing well-defined interfaces to other components.
- Components encapsulate concepts by hiding details from other components.





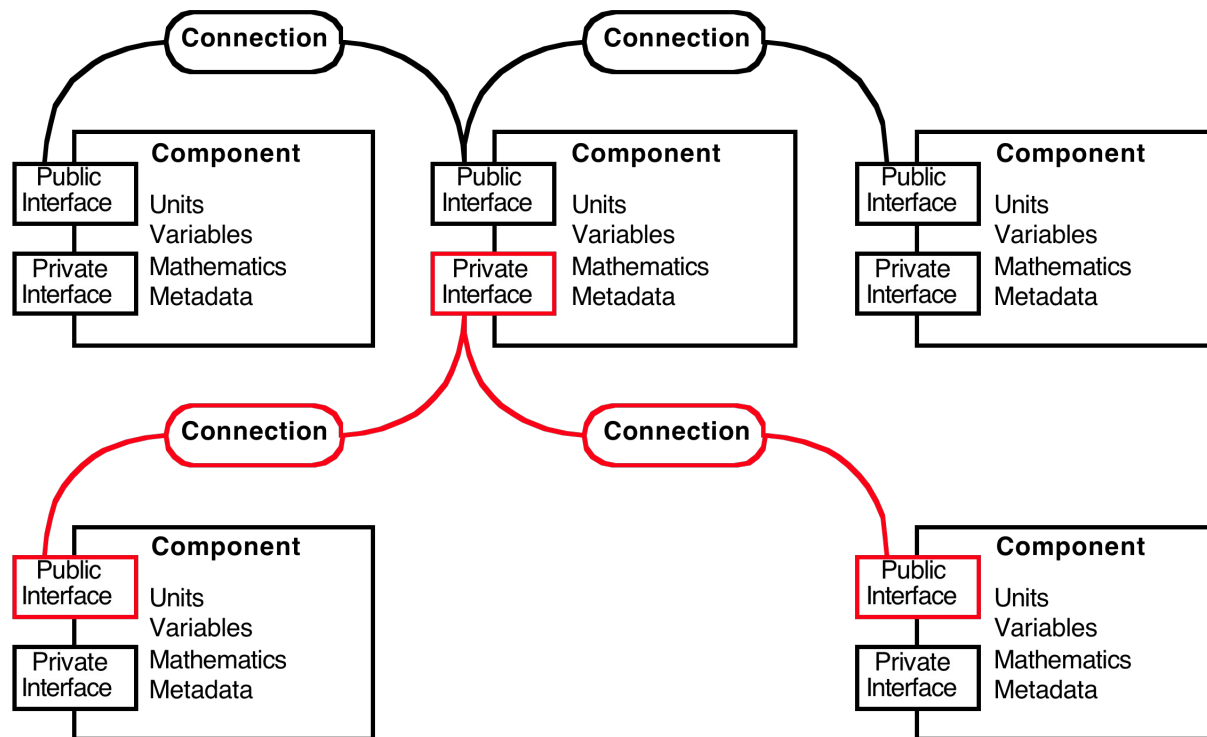
# CellML connections

- *Connections* provide the means for sharing information by associating variables visible in the interface of one component with those in the interface of another component.
- Consistency is enforced by requiring that all variables be assigned appropriate physical *units*.



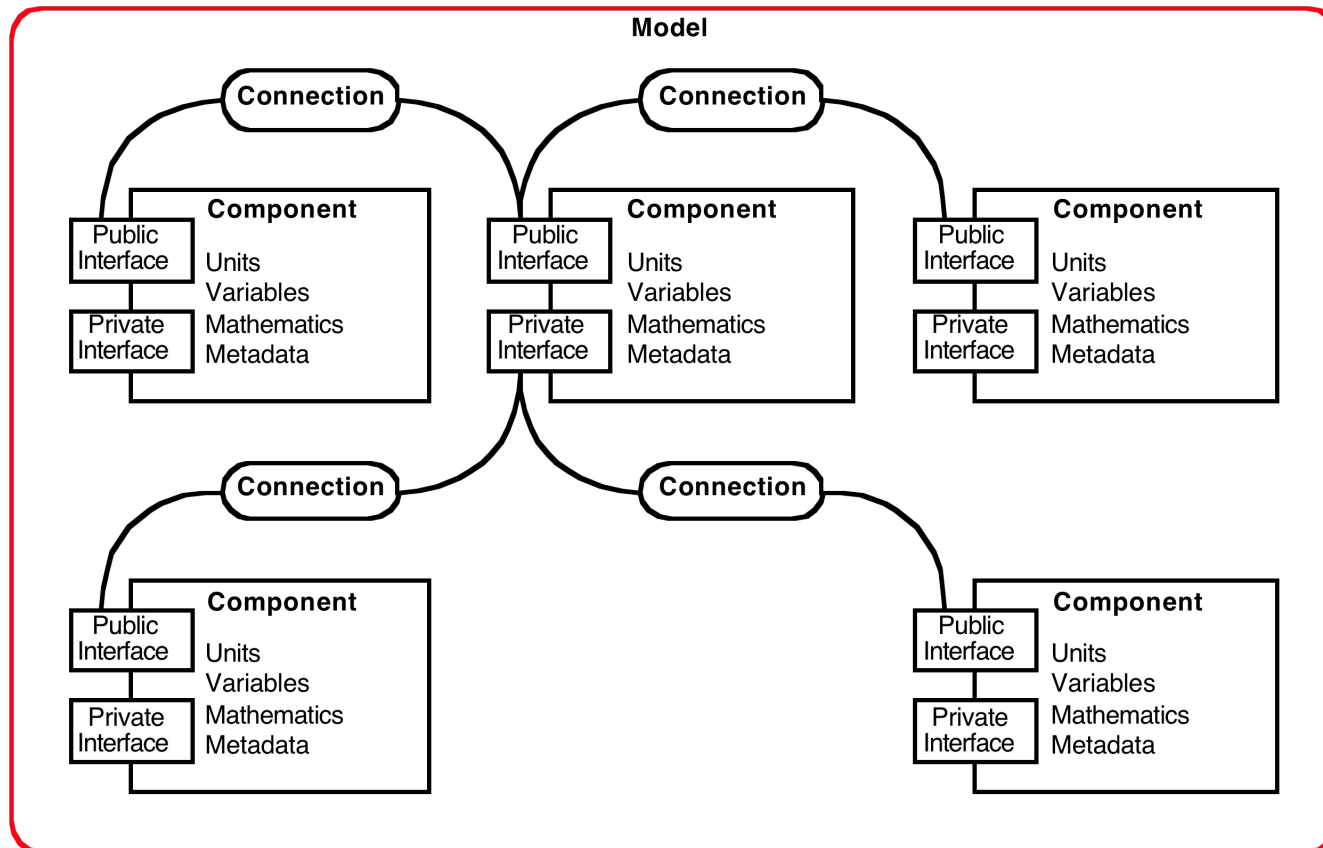
# CellML encapsulation

- Encapsulation hierarchies are enabled using *private interfaces*.



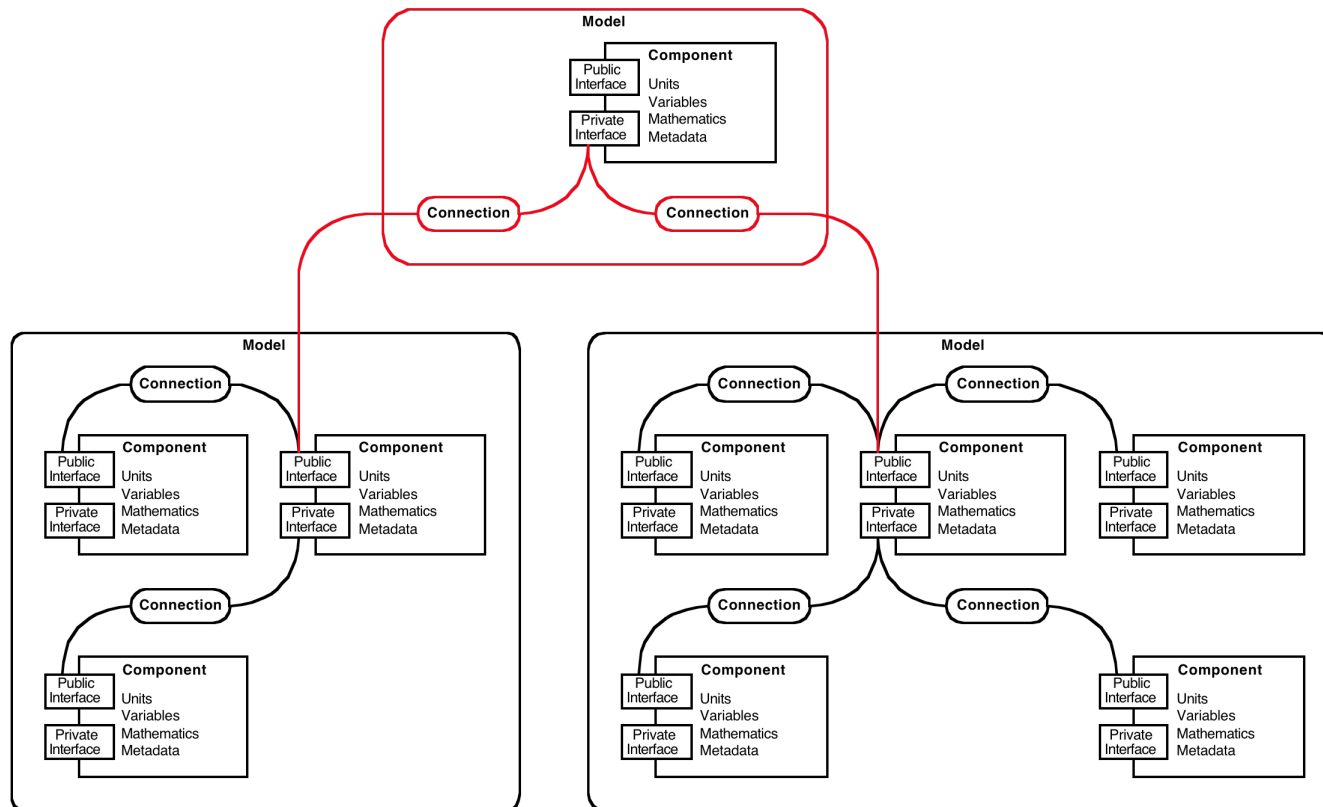
# CellML model

- A *model* is the root element for a CellML document. It is a container for components, connections, units, and metadata.



# CellML import

- Model reuse is enabled by the *import* element.
- New models may thus be constructed by combining existing models into model hierarchies.



# Model libraries

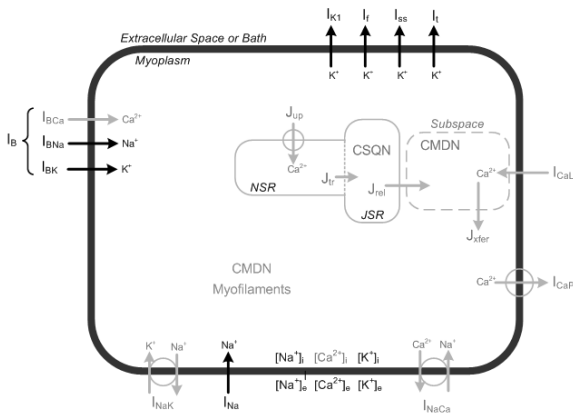
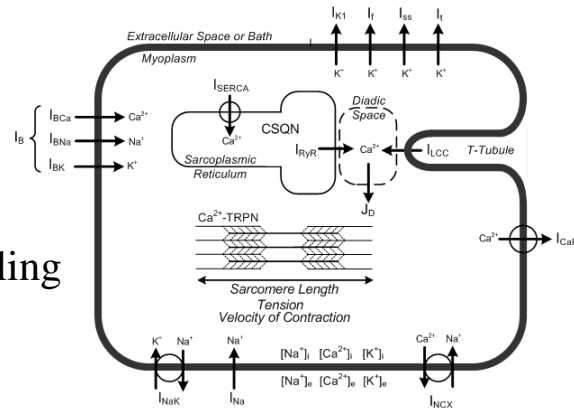
- Model reuse encourages the creation of model libraries.
- This is possible in CellML because there is no distinction between models as stand-alone entities and models as templates.
- Every import creates a new instance of the imported model in the importing model.
- The same model can be imported multiple times to create separate instances (with distinct identifiers) within the importing model.

# Model libraries

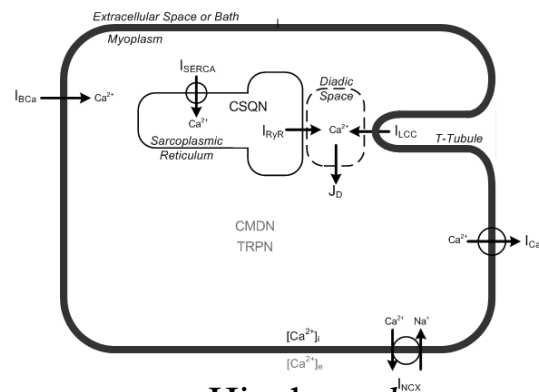
- Obvious candidates for reuse are existing CellML 1.0 models available in the model repository.
- Other candidates are the decomposition of existing models by identifying reusable generic (sub)models.
- These generic models are then formulated as new library models, making them available as basic building blocks for import into larger models.
- Useful generic models include collections of:
  - units (complicated combinations, non-SI definitions)
  - constants (codata fundamental physical constants)
  - processes (integrators, reactions, rate relations, ion channels, ...)
- Sometimes difficult to balance genericity versus conciseness.

# Combine models using CellML import

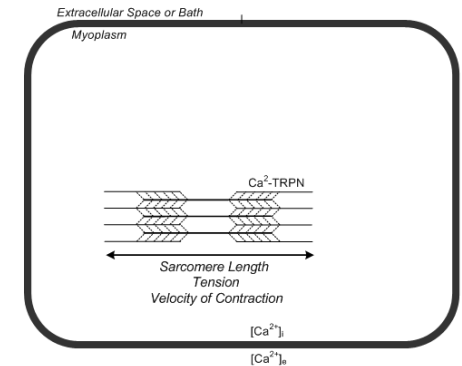
Terkildsen *et al.*  
Integrated model of e-c coupling



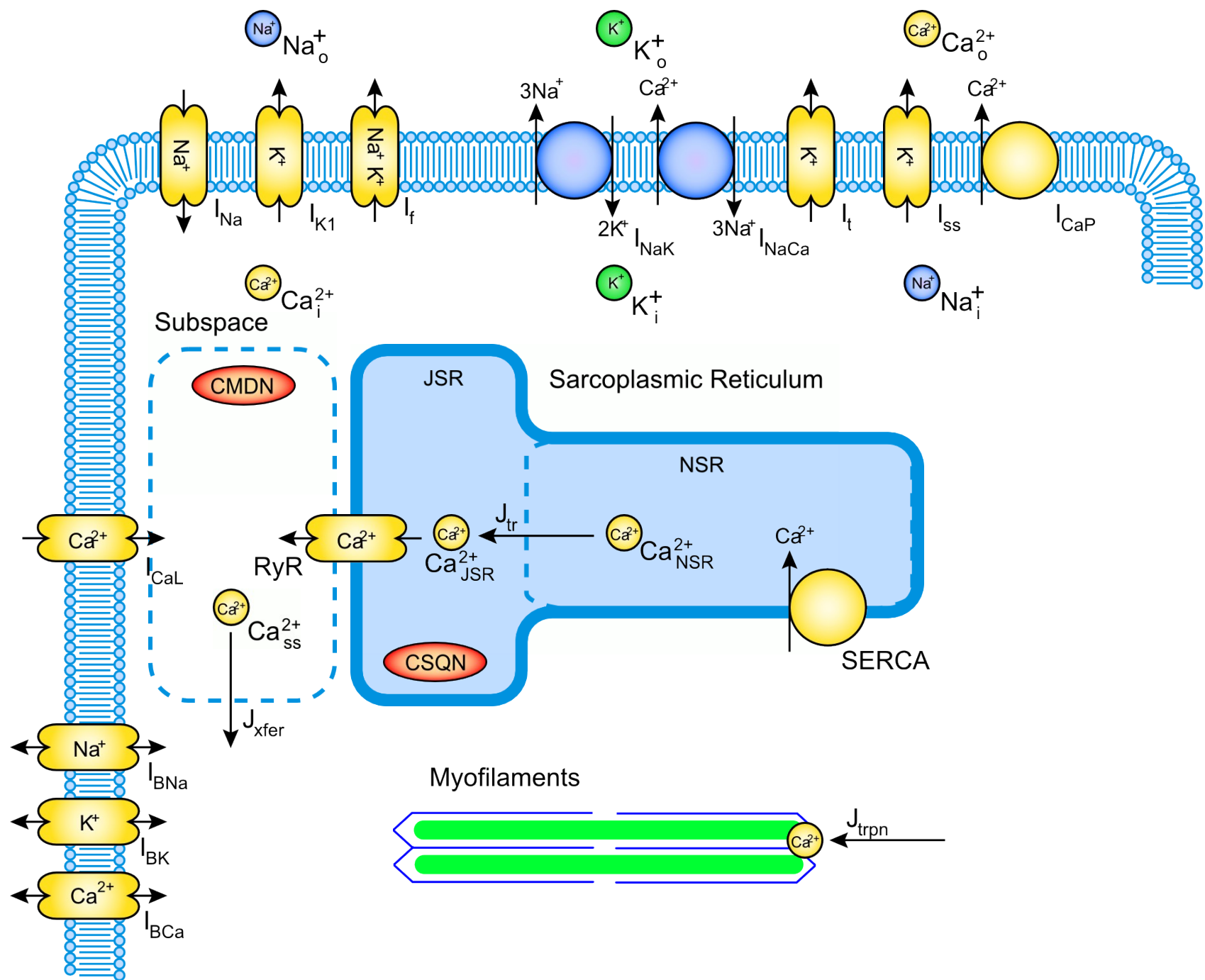
Pandit *et al.*  
cardiac action potential



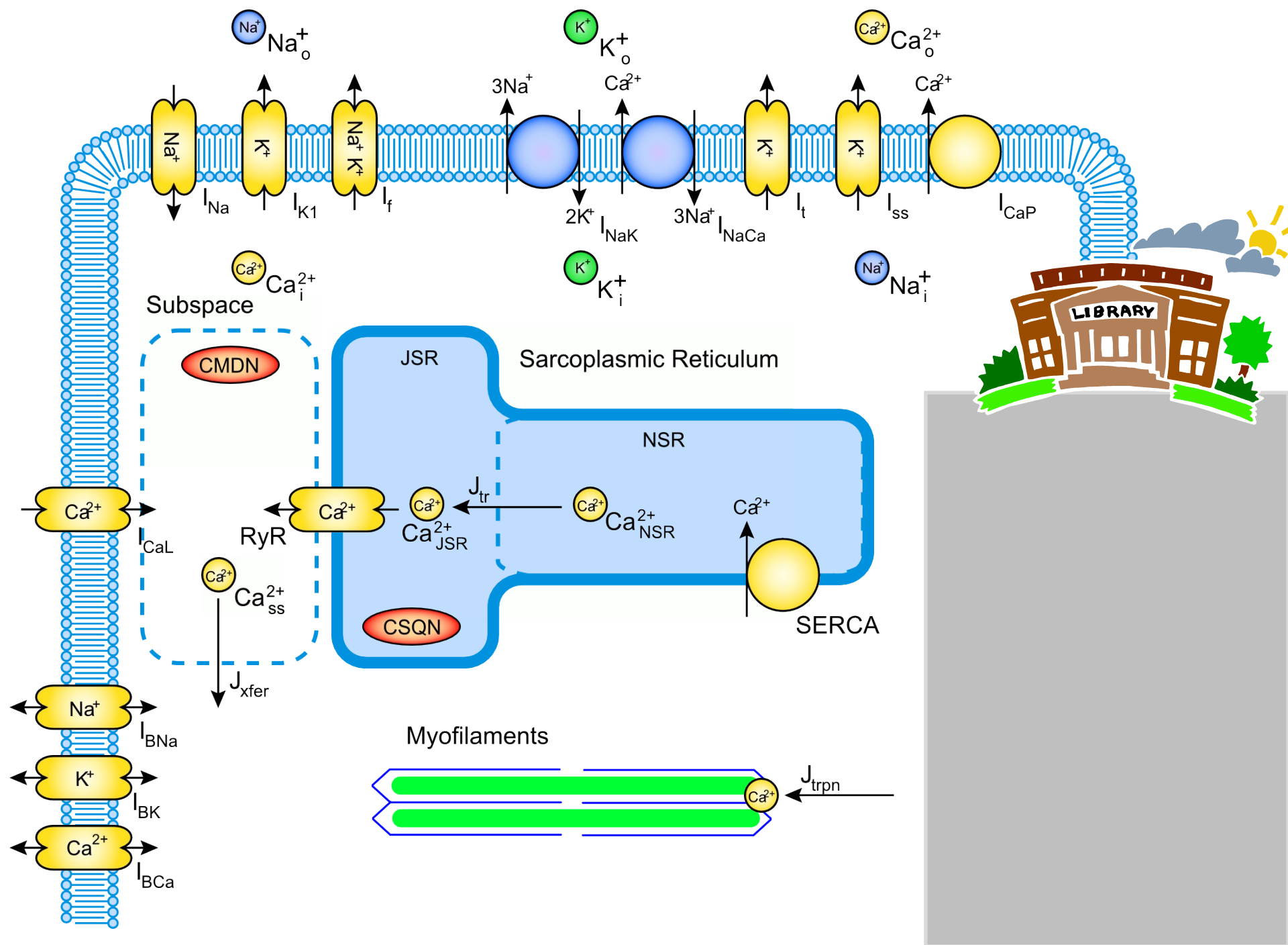
Hinch *et al.*  
Ca-induced Ca release

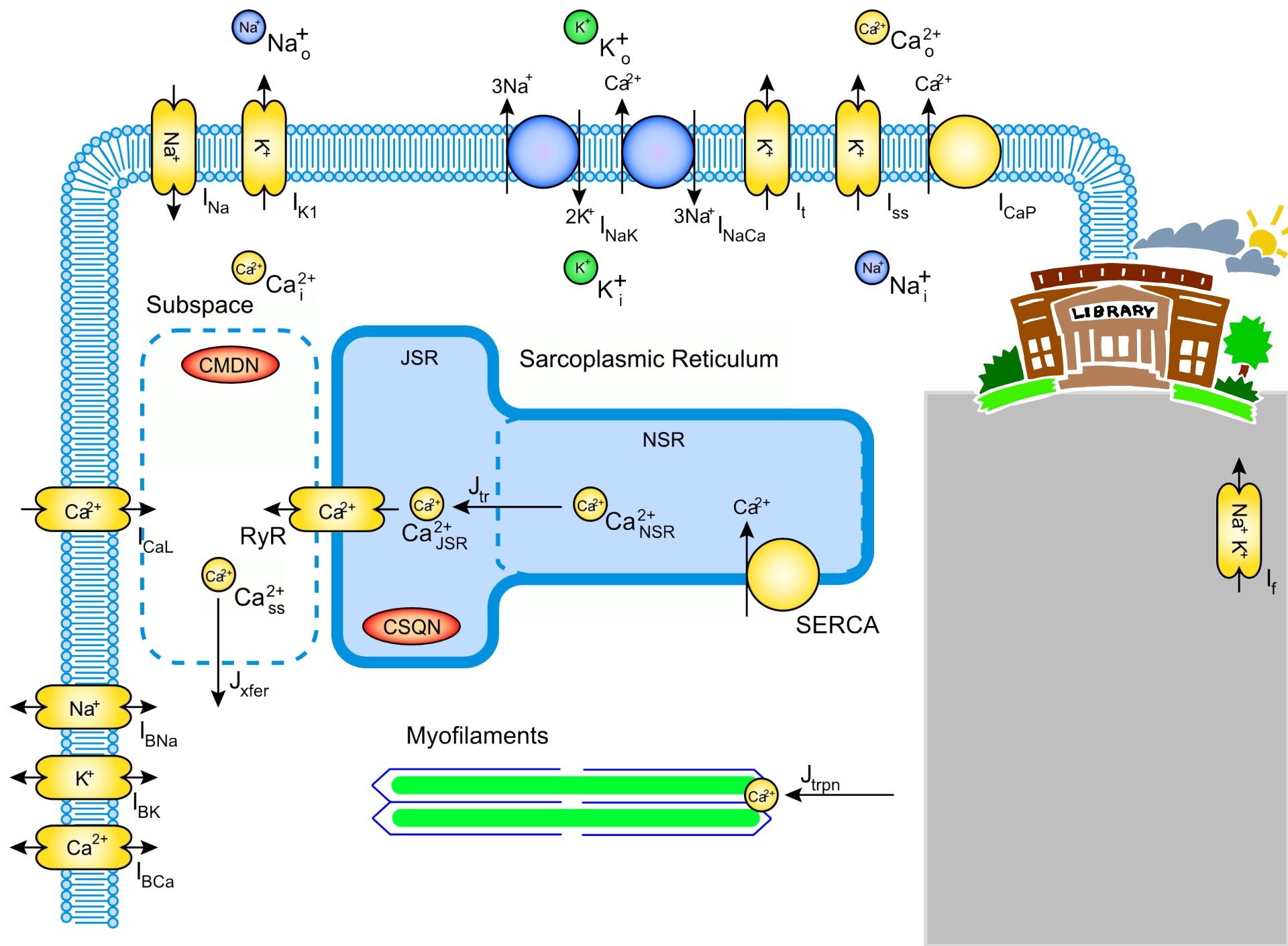


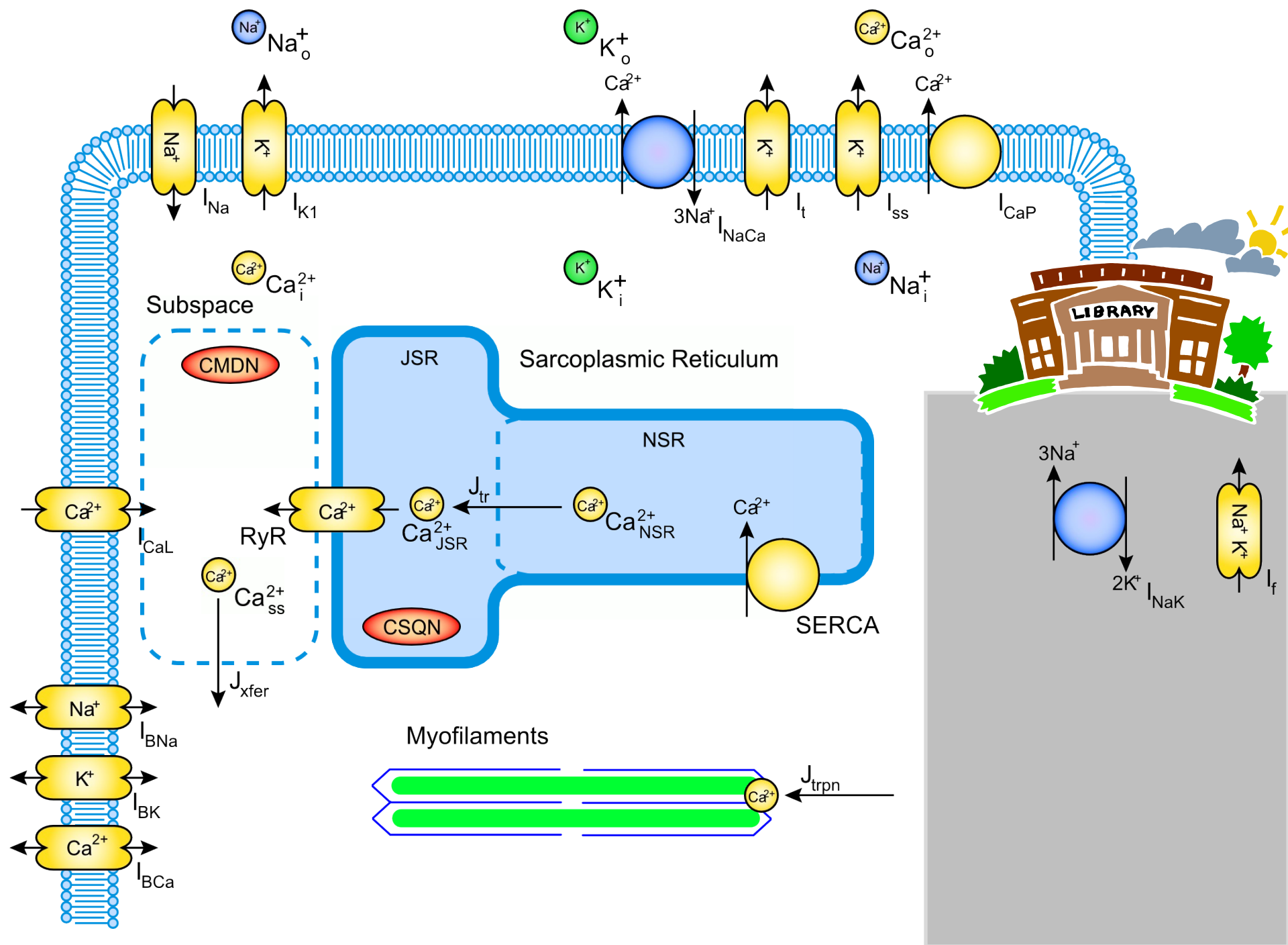
Niederer *et al.*  
myofilament mechanics

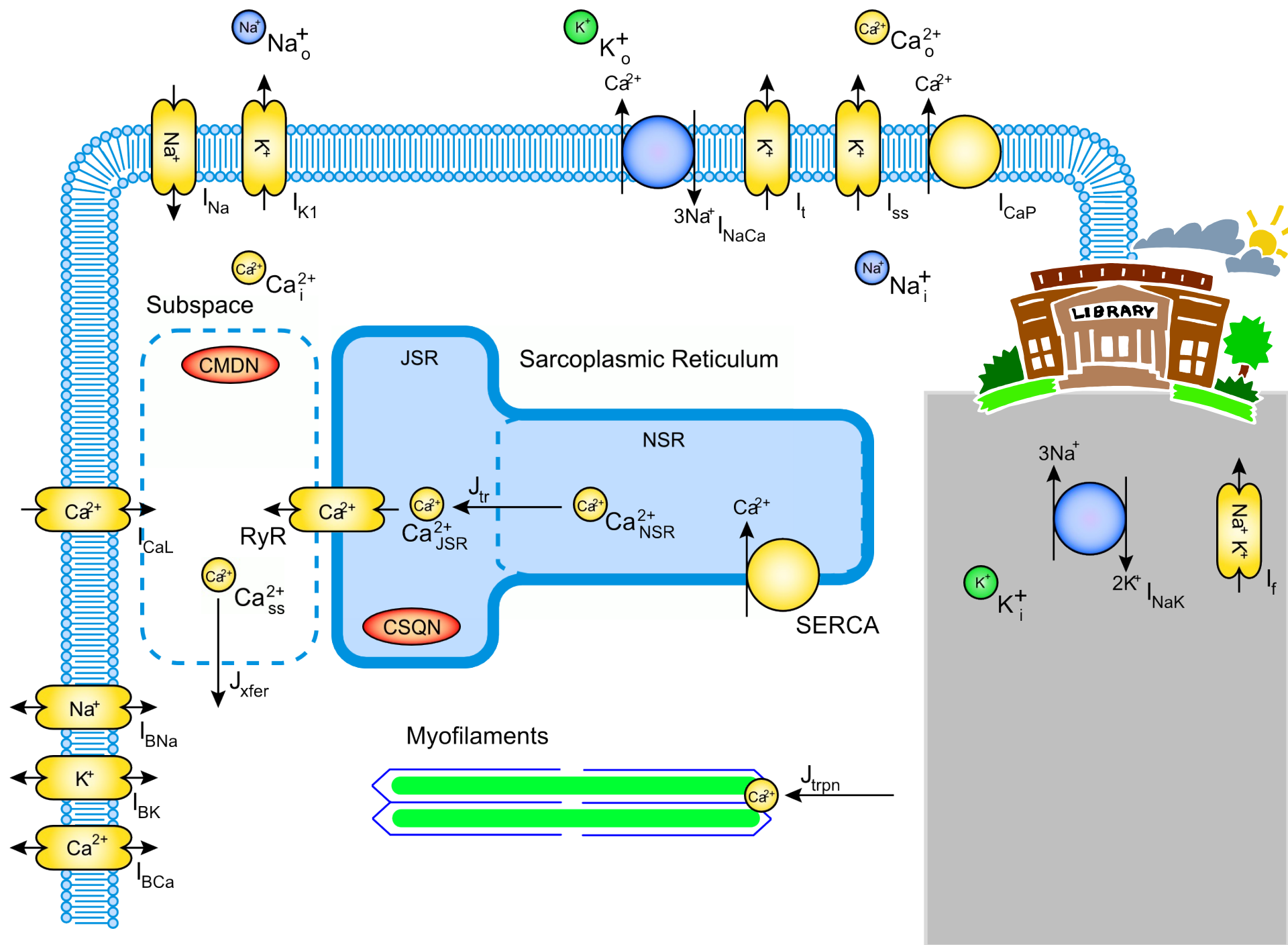


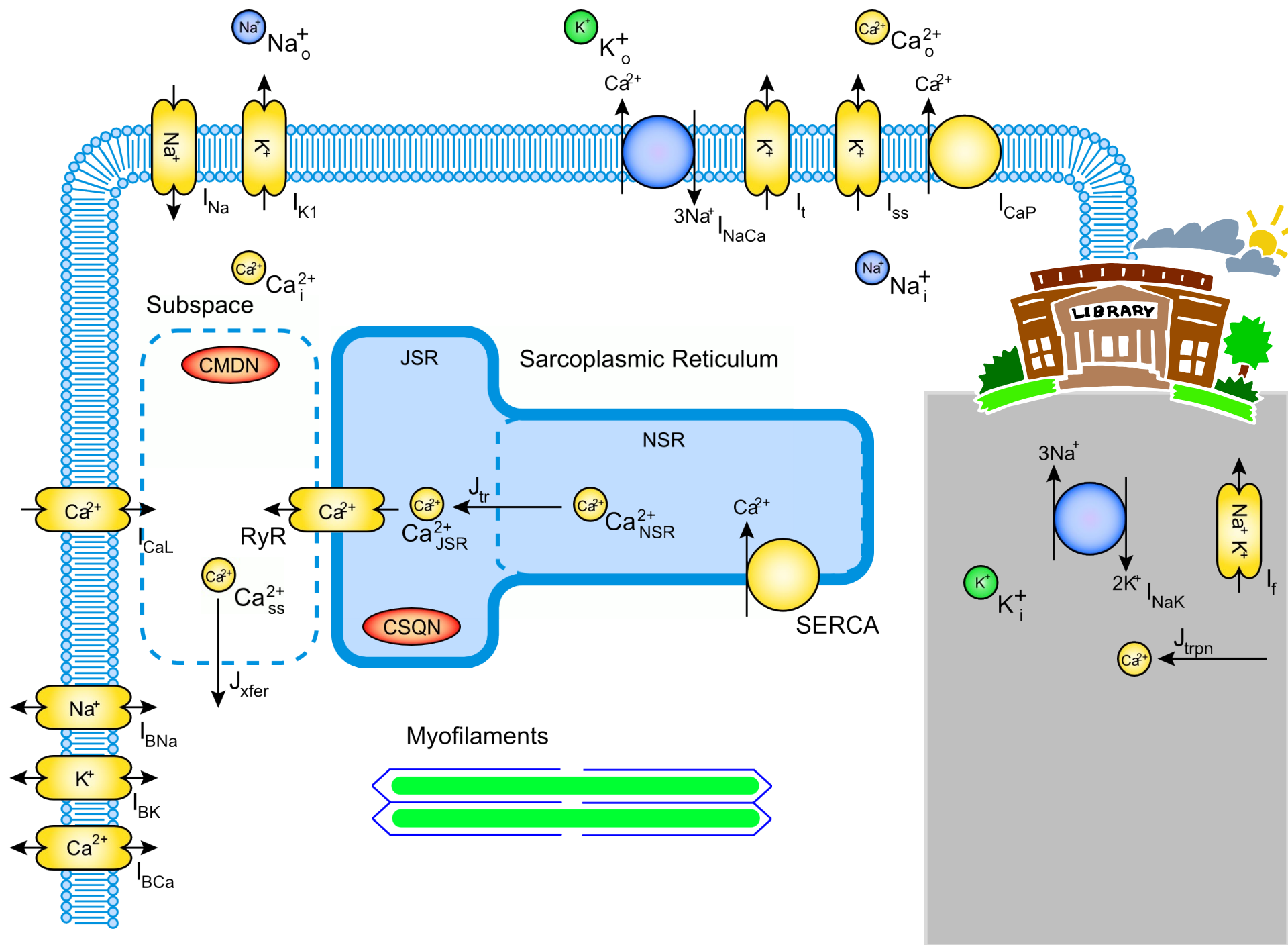


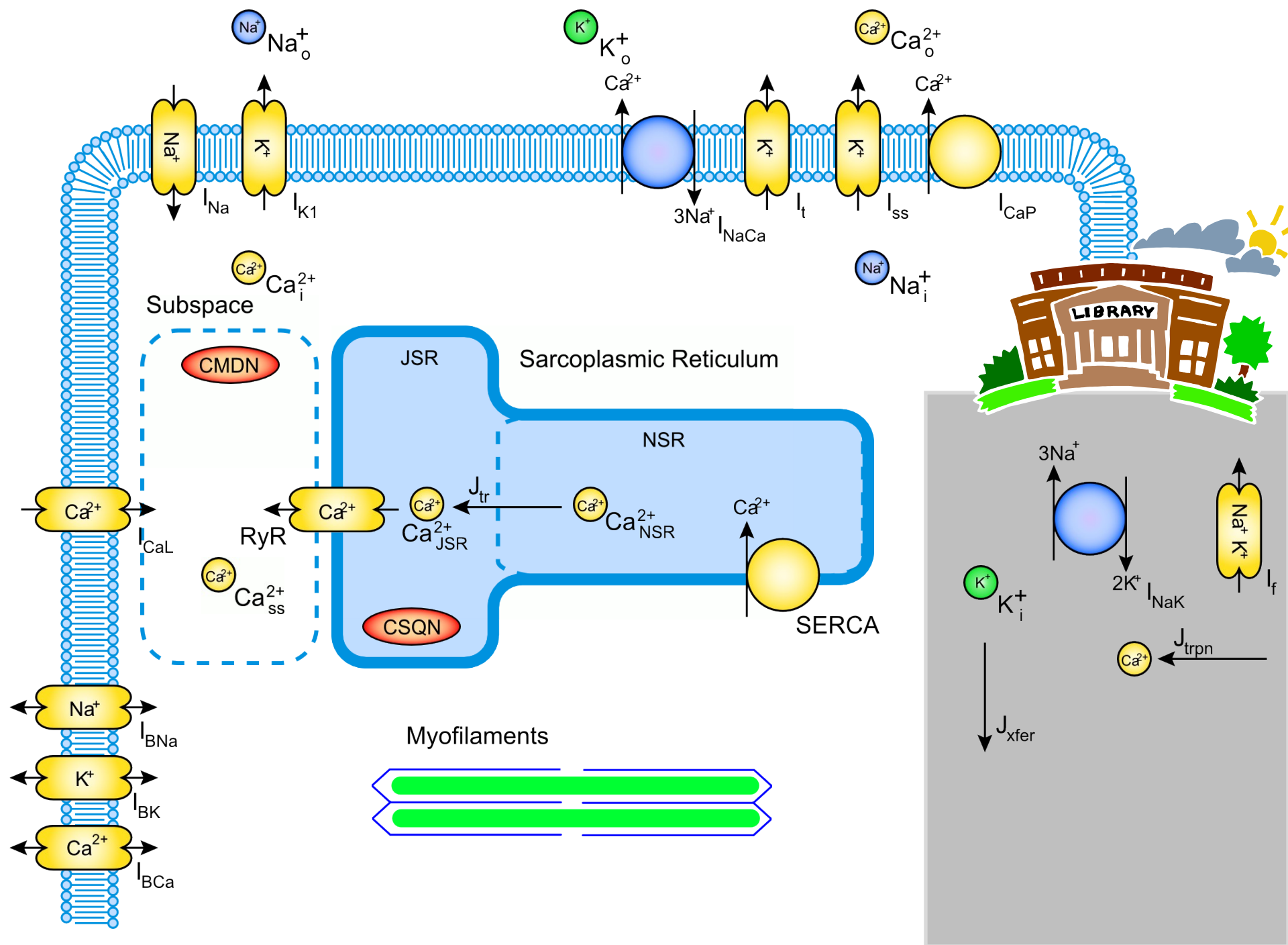


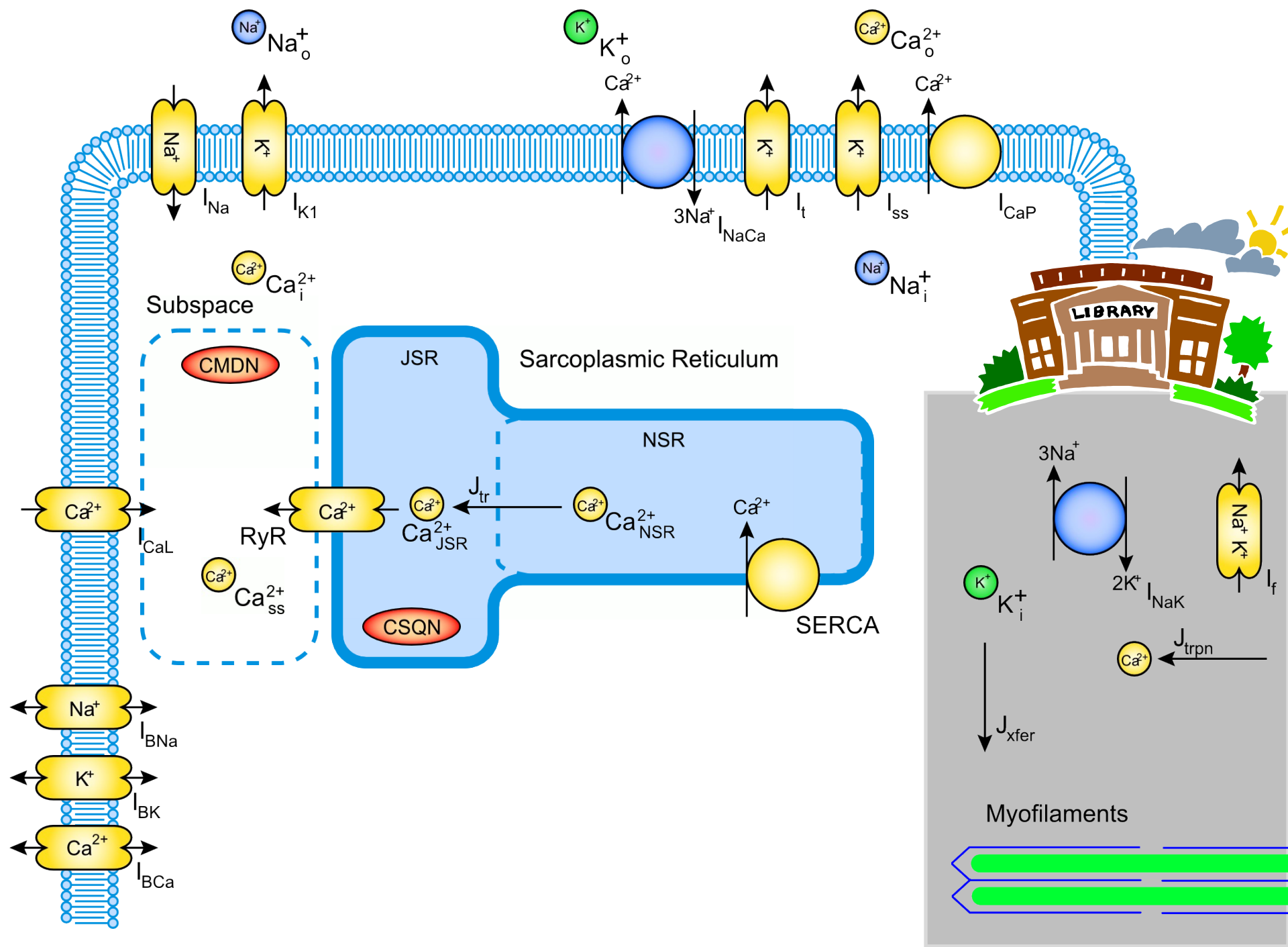
















# Best practice

- Most useful non-trivial library components describe clearly identifiable biophysical processes.
- Sarala Wimilaratne has given several examples of this approach in her PhD thesis on CellML model visualisation (Cooling 07 GCPR cycle, Hodgkin-Huxley 52, Nobel 62).
- We are compiling a list of best-practice examples based on the experience gained through the process of model decomposition.
- This work is still in its early stages – there is still much to be learned about which approaches offer the best long-term benefits.

# Best practice

- Put reusable mathematics in separate components, and use *<import>*s to instantiate these for use where appropriate.
- Use ‘*\_delta*’ components to extensibly connect multiple fluxes to species of interest.
- Use separate conversion components for connections where applicable.
- Build coarse-grained components from aggregations of finer-grained, biologically atomic components.
- Define *<units>* at the lowest level possible, *<import>*ing into higher level components as necessary.
- Separate out all parameter values into one or more non-mathematical CellML documents.
- Universal constants should be *<import>*ed from a non-mathematical CellML document (a standard based document on [UC] is recommended).
- If encapsulating, expose all potentially useful values using *public\_interface=“out”*.



# Physiome

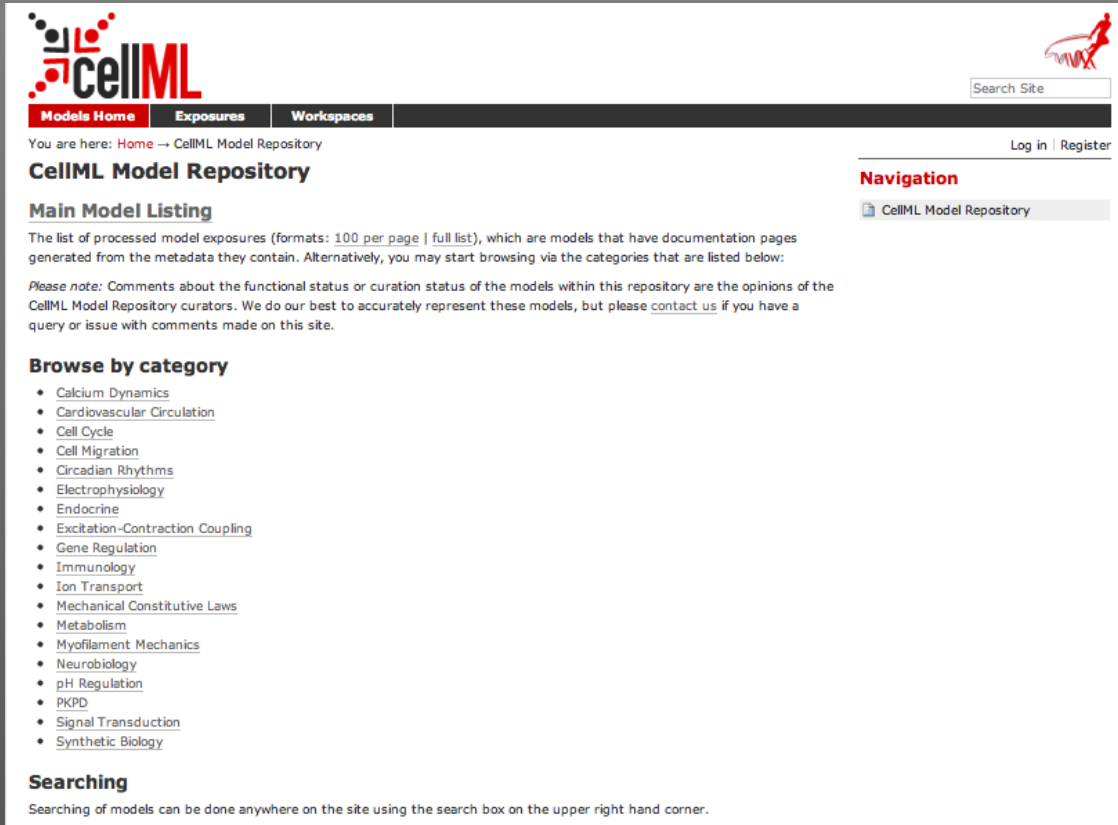
## The CellML Model Repository and Model Curation

Dr Catherine Lloyd  
Senior Database Curator  
Auckland Bioengineering Institute



# The CellML model repository

<http://models.cellml.org>



The screenshot shows the homepage of the CellML Model Repository. At the top left is the CellML logo, and at the top right is a search box labeled "Search Site". Below the logo is a navigation bar with "Models Home", "Exposures", and "Workspaces". The main content area features a breadcrumb trail "You are here: Home → CellML Model Repository", a "Log in | Register" link, and a "Navigation" section with a link to "CellML Model Repository". The "Main Model Listing" section includes a description of processed model exposures and a "Browse by category" list with 18 items: Calcium Dynamics, Cardiovascular Circulation, Cell Cycle, Cell Migration, Circadian Rhythms, Electrophysiology, Endocrine, Excitation-Contraction Coupling, Gene Regulation, Immunology, Ion Transport, Mechanical Constitutive Laws, Metabolism, Myofilament Mechanics, Neurobiology, pH Regulation, PKPD, Signal Transduction, and Synthetic Biology. A "Searching" section at the bottom explains that models can be found using the search box in the upper right corner.

Began life as a set of test cases

- Today contains >500 models
- Most the models are derived from published papers
- All the models are free for download



# Model categories include

signal transduction

electrophysiology

calcium dynamics

metabolism


cell cycle

muscle contraction

immunology

synthetic biology

# How to find a model



goldbeter 1991

Search results...

- Goldbeter, 1991** [100%]
- Dupont Berridge Goldbeter 199...** [99%]
- A theory for controlling cell...** [87%]  
A theory for controlling cell cycle dynamics using a reversibly binding inhibitor
- A Minimal Cascade Model for t...** [79%]  
A Minimal Cascade Model for the Mitotic Oscillator Involving Cyclin and cdc2 Kinase
- A Minimal Cascade Model for t...** [79%]  
A Minimal Cascade Model for the Mitotic Oscillator Involving Cyclin and cdc2 Kinase
- A theory for controlling cell...** [70%]  
A theory for controlling cell cycle dynamics using a reversibly binding inhibitor
- A theory for controlling cell...** [70%]  
A theory for controlling cell cycle dynamics using a reversibly binding inhibitor
- Signal-induced Ca<sup>2+</sup> oscillati...** [66%]  
Signal-induced Ca<sup>2+</sup> oscillations: Properties of a model based on (Ca<sup>2+</sup>)-induced Ca<sup>2+</sup> release

## Browse by category

- [Calcium Dynamics](#)
- [Cardiovascular Circulation](#)
- [Cell Cycle](#)
- [Cell Migration](#)
- [Circadian Rhythms](#)
- [Electrophysiology](#)
- [Endocrine](#)
- [Excitation-Contraction Coupling](#)
- [Gene Regulation](#)
- [Immunology](#)
- [Ion Transport](#)
- [Mechanical Constitutive Laws](#)
- [Metabolism](#)
- [Myofilament Mechanics](#)
- [Neurobiology](#)
- [pH Regulation](#)
- [PKPD](#)
- [Signal Transduction](#)
- [Synthetic Biology](#)

The repository is more than just a storage system

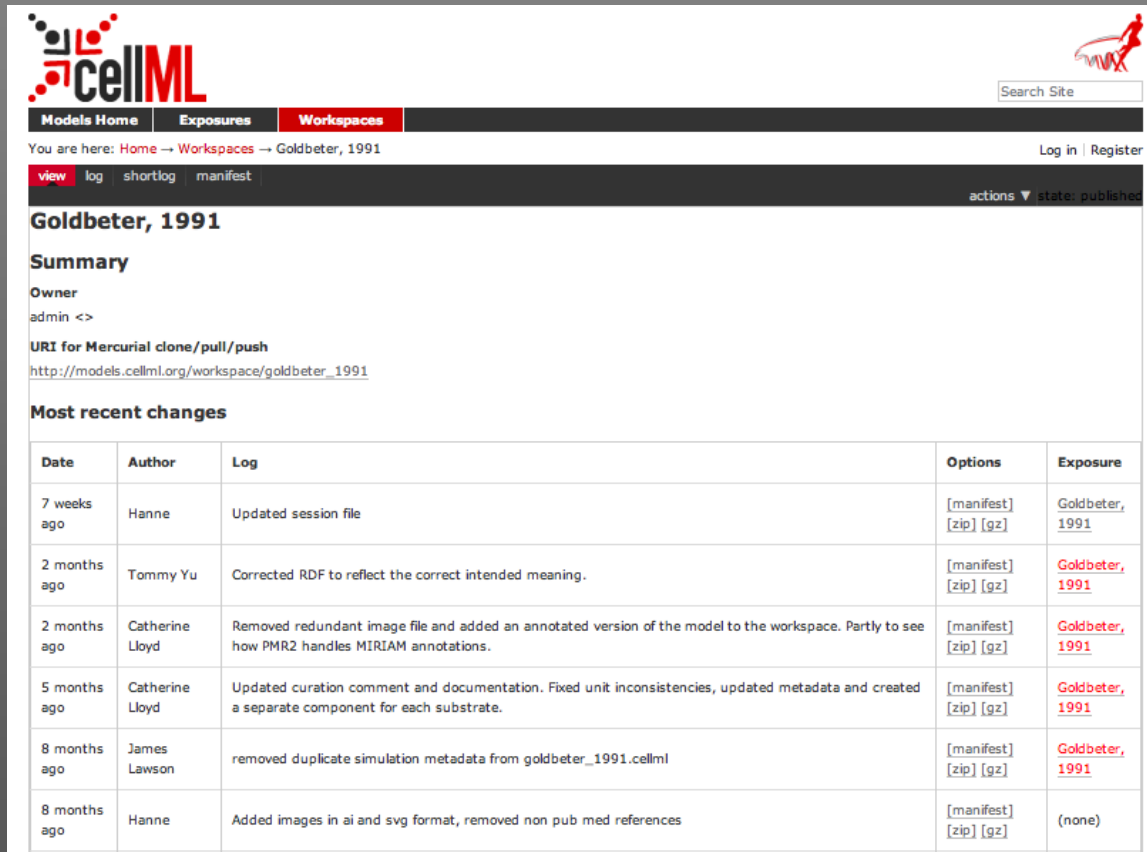




It's designed to facilitate model  
exchange and reuse



# Workspace and change-history



The screenshot shows the CellML website interface. At the top left is the CellML logo. To the right is a search box. Below the logo is a navigation bar with links for 'Models Home', 'Exposures', and 'Workspaces'. The current page is 'Goldbeter, 1991'. Below the navigation bar is a breadcrumb trail: 'You are here: Home → Workspaces → Goldbeter, 1991'. There are also links for 'Log in' and 'Register'. Below the breadcrumb trail are links for 'view', 'log', 'shortlog', and 'manifest'. At the bottom right of the navigation bar are 'actions' and 'state: published'. The main content area is titled 'Goldbeter, 1991' and has a 'Summary' section. The summary includes the owner 'admin <>', the URI for Mercurial clone/pull/push, and a link to the workspace. Below the summary is a section for 'Most recent changes' which contains a table of changes.

| Date         | Author          | Log                                                                                                                                           | Options                  | Exposure           |
|--------------|-----------------|-----------------------------------------------------------------------------------------------------------------------------------------------|--------------------------|--------------------|
| 7 weeks ago  | Hanne           | Updated session file                                                                                                                          | [manifest]<br>[zip] [gz] | Goldbeter,<br>1991 |
| 2 months ago | Tommy Yu        | Corrected RDF to reflect the correct intended meaning.                                                                                        | [manifest]<br>[zip] [gz] | Goldbeter,<br>1991 |
| 2 months ago | Catherine Lloyd | Removed redundant image file and added an annotated version of the model to the workspace. Partly to see how PMR2 handles MIRIAM annotations. | [manifest]<br>[zip] [gz] | Goldbeter,<br>1991 |
| 5 months ago | Catherine Lloyd | Updated curation comment and documentation. Fixed unit inconsistencies, updated metadata and created a separate component for each substrate. | [manifest]<br>[zip] [gz] | Goldbeter,<br>1991 |
| 8 months ago | James Lawson    | removed duplicate simulation metadata from goldbeter_1991.cellml                                                                              | [manifest]<br>[zip] [gz] | Goldbeter,<br>1991 |
| 8 months ago | Hanne           | Added images in ai and svg format, removed non pub med references                                                                             | [manifest]<br>[zip] [gz] | (none)             |

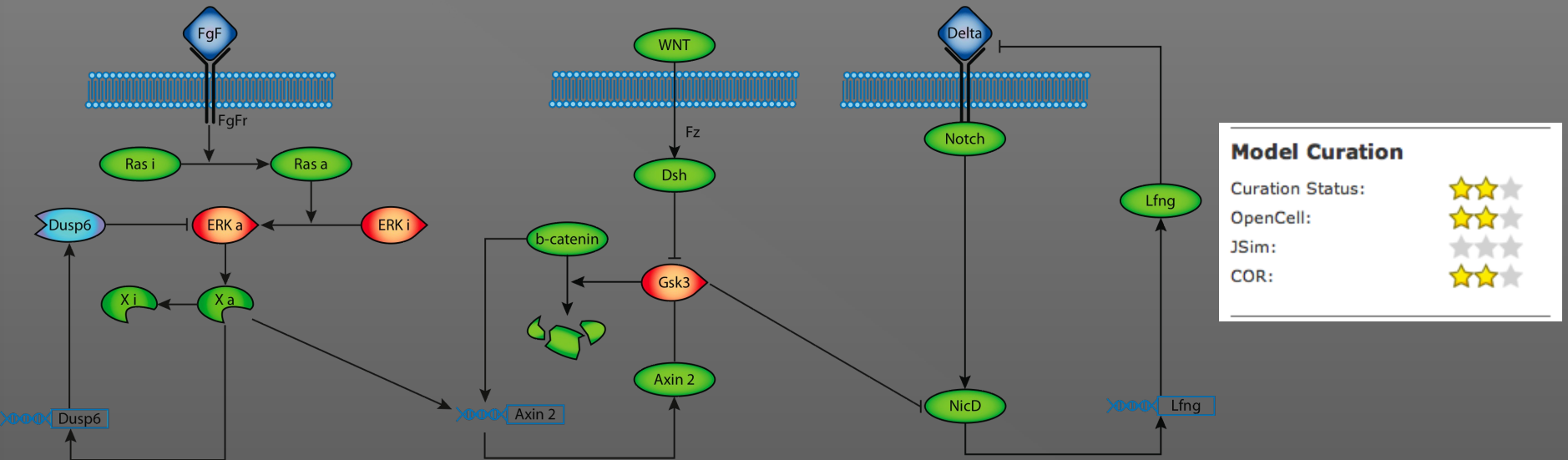
- Each model and its associated files are stored together in a **workspace**

- Every alteration is recorded and time-stamped to provide a detailed **change-history**

# Exposure

Goldbeter, Pourquie, 2008

Modeling the segmentation clock as a network of coupled oscillations in the Notch, Wnt and FGF signaling pathways



Modeling the segmentation clock as a network of coupled oscillations in the Notch, Wnt and FGF signaling pathways, Albert Goldbeter and Olivier Pourquie, 2008, *Journal of Theoretical Biology*, 252, 574-585. [PubMed ID: 18308339](https://pubmed.ncbi.nlm.nih.gov/18308339/)

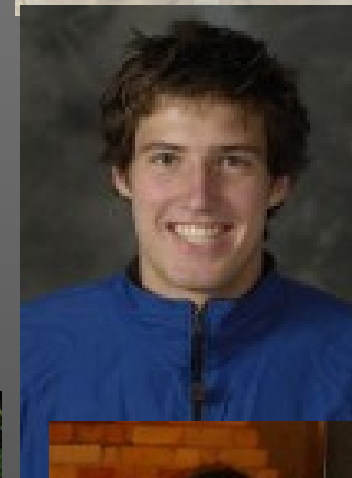
- Each model entry may be accompanied by an abstract, curation status, citation, and a schematic diagram.

# Who is submitting the models?

Curators



- Modellers



- Curators & modellers together



# Curation



- Curation involves model validation & annotation
- A star system denotes the curation status of a model
- There's also a more detailed model status comment on display, and the change-history comments recorded in the workspace

## Model Status

This CellML model runs in both PCEnv and COR to recreate the published results. The units have been checked and they are consistent. In this particular version of the model couples the Notch, Wnt and FGF signalling pathways together and so uses equations A17 and A18 in the appendix to replace equations A4 and A10 respectively.

# Why curate models?

FACT: Of the ~500 models in the repository only a small handful have been directly translated from the published paper into a working CellML model

- QUOTE: *“As anyone who has tried to reproduce a published mathematical model will testify, it’s a long, tedious, and generally futile task. Equations are replaced by ambiguous descriptions, parameter values are left undefined and, worst of all, the main author has given up science to set up a vegan cup-cake business.”* Dr K. S.

Where are things heading?

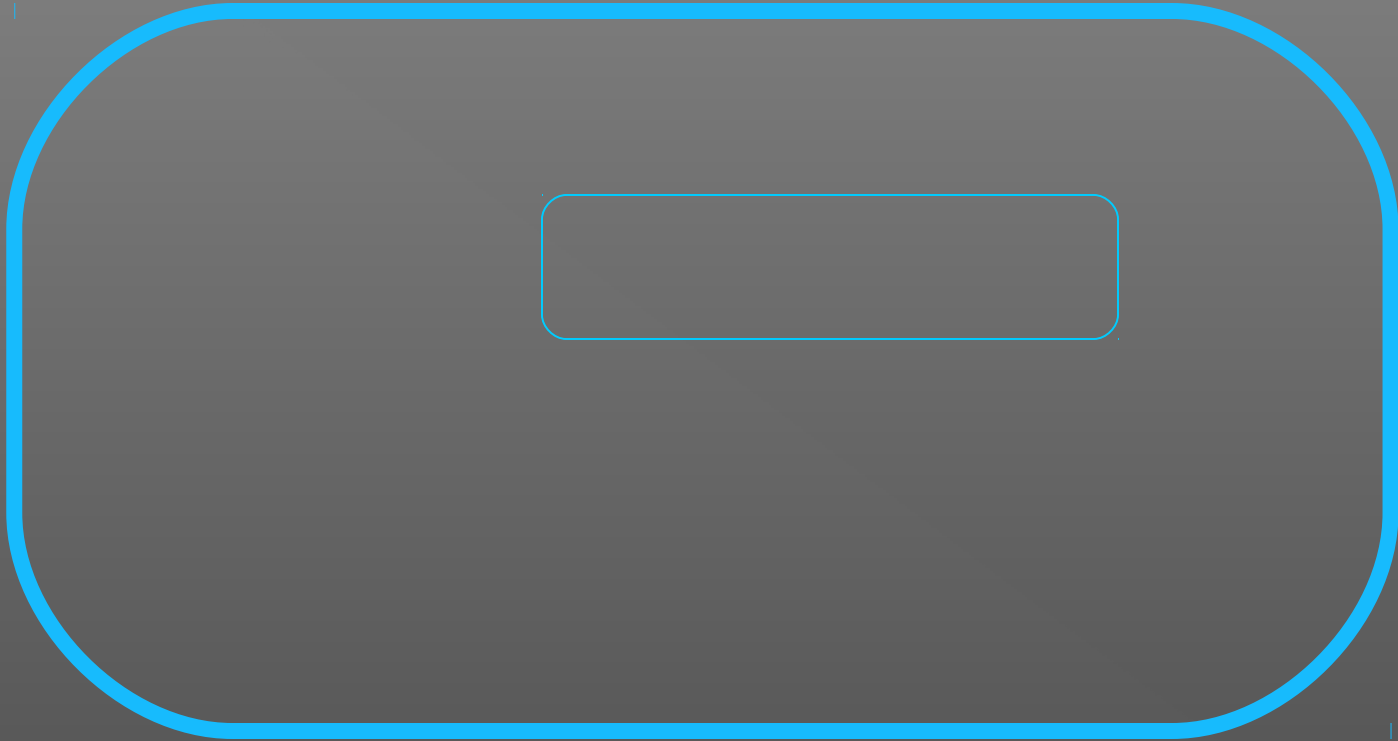


# A library of smaller models

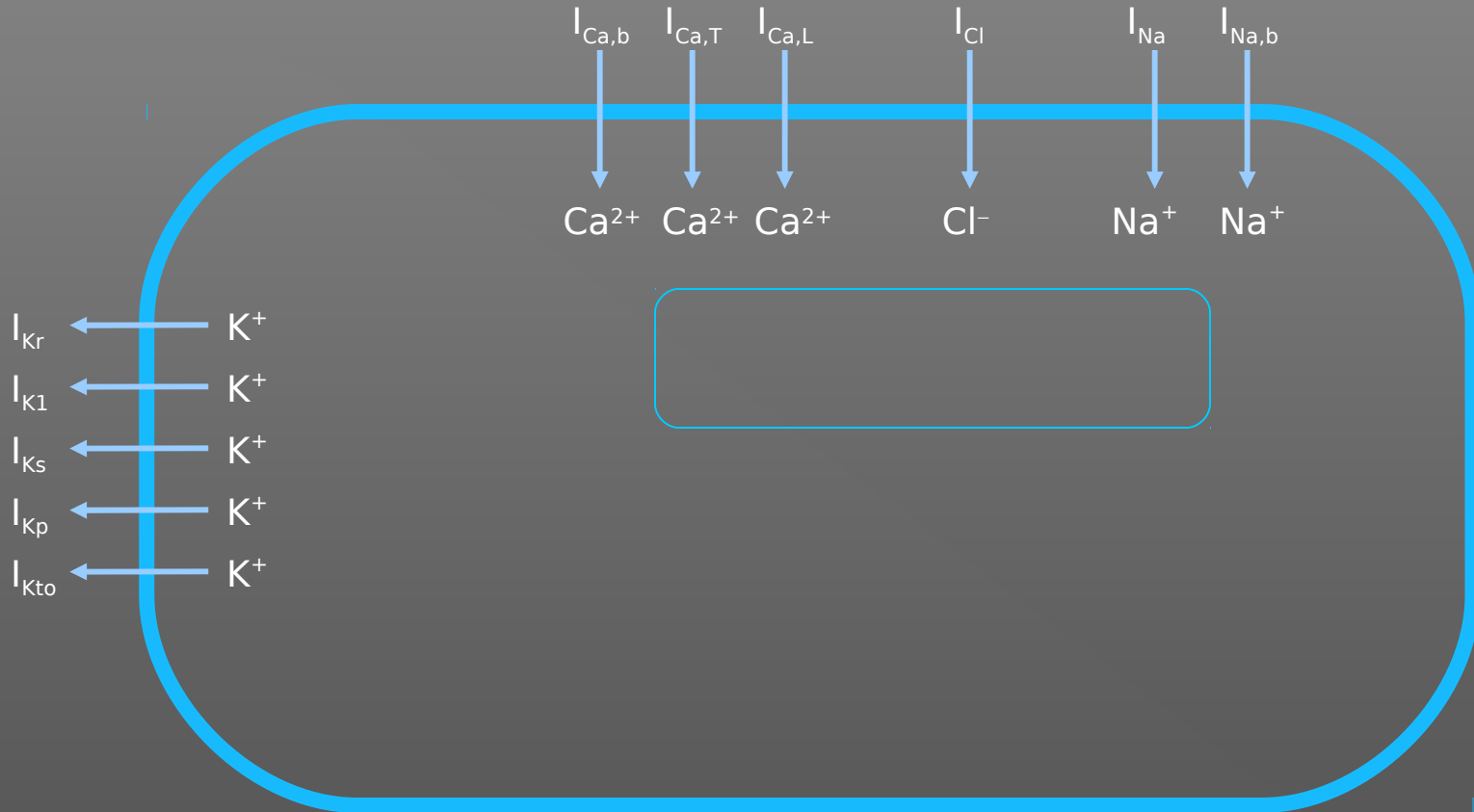




# A library of smaller models

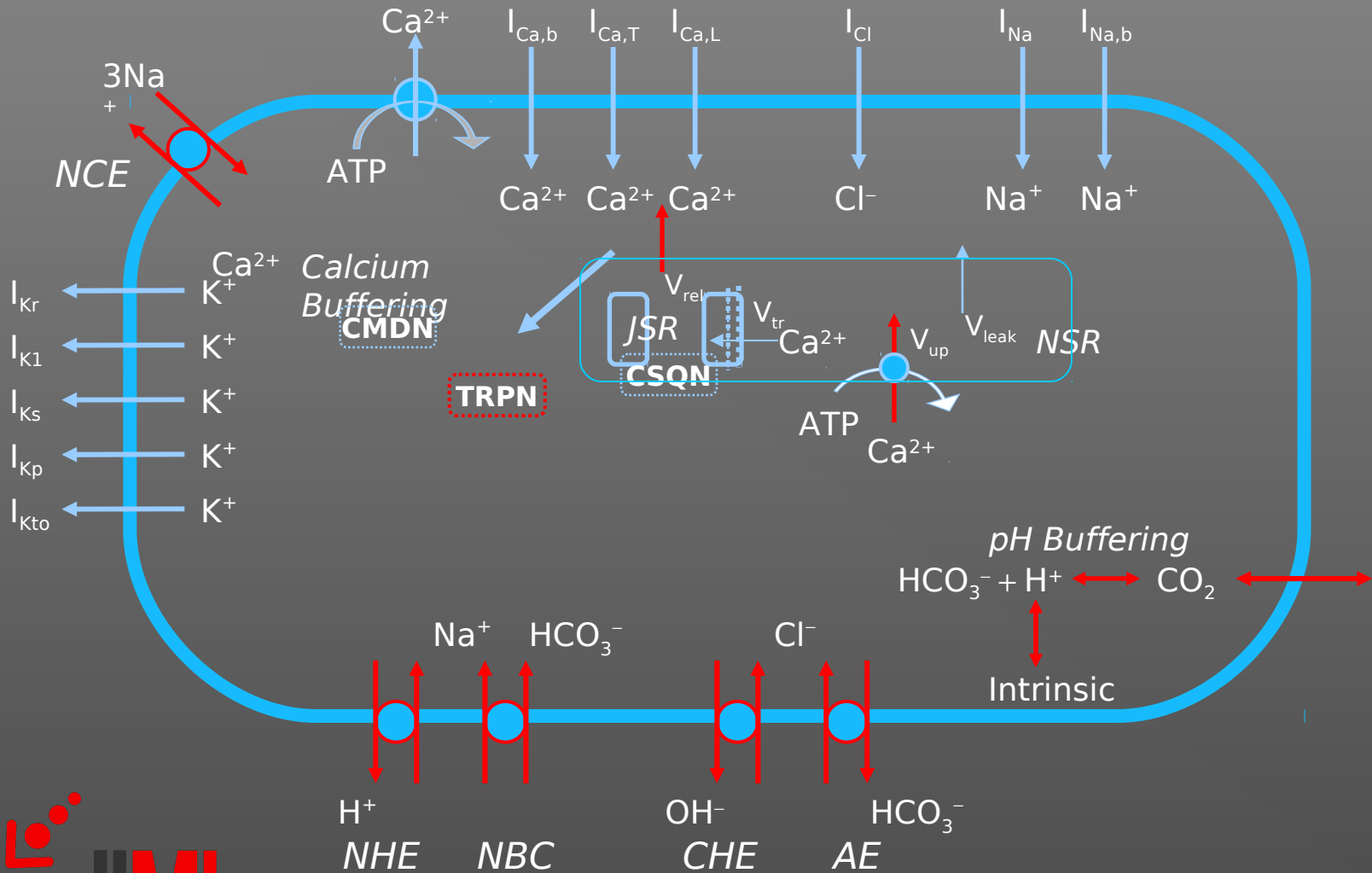


# A library of smaller models





# A library of smaller models

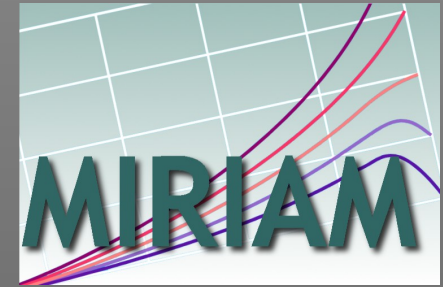
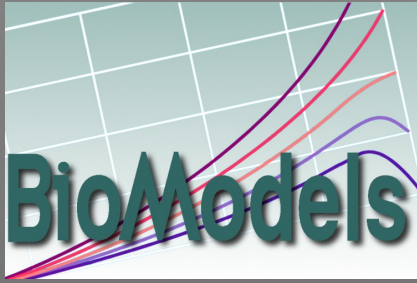


# Model annotation

```
<component cmeta:id="M_star" name="M_star">
  <rdf:RDF xmlns:rdf="http://www.w3.org/1999/02/22-rdf-syntax-ns#">
    <rdf:Description rdf:about="#M_star">
      <dc:title>M_star</dc:title>
      <dcterms:alternative>fraction of inactive cdc2 kinase</dcterms:alternative>
    </rdf:Description>
  </rdf:RDF>
  <variable units="dimensionless" public_interface="out" name="M_star" cmeta:id="M_M_" >
    <rdf:RDF xmlns:rdf="http://www.w3.org/1999/02/22-rdf-syntax-ns#" xmlns:dc="http://purl.org/dc/elements/1.1/"
      xmlns:dcterms="http://purl.org/dc/terms/" xmlns:bqbiol="http://biomodels.net/biology-qualifiers/" xmlns:bqmodel="http://
      biomodels.net/model-qualifiers/">
      <rdf:Description rdf:about="#M_M_">
        <bqbiol:isVersionOf>
          <rdf:Bag>
            <rdf:li rdf:resource="urn:miriam:uniprot:P24033"/>
            <rdf:li rdf:resource="urn:miriam:uniprot:P35567"/>
            <rdf:li rdf:resource="urn:miriam:obo.sbo:sbo%3A0000252"/>
          </rdf:Bag>
        </bqbiol:isVersionOf>
      </rdf:Description>
    </rdf:RDF>
  </variable>
```

- Labelling the models with biological & biophysical data
- Using consistent terms from ontologies
- For improved repository searches, facilitated language interconversion, and model visualisation

# Common curation standards



MIRIAM – The Minimal Information Required in the Annotation of Models

- MIRIAM provides a list of criteria a model must satisfy to become fully curated
- By replacing the “stars” with MIRIAM-based “flags” the curation status of a model becomes less ambiguous





**Physiome model repository**  
**[models.physiomeproject.org](http://models.physiomeproject.org)**


Physiome Model Repository — CellML Model Repository - Mozilla Firefox

File Edit View History Bookmarks Tools Help

http://models.physiomeproject.org/welcome

Google

Physiome Model Repository... Andre's Hodgkin Huxley mo... PMR2 basic tutorial draft — ...



Search Site

Models Home Exposures Workspaces

You are here: Home → Physiome Model Repository

## Physiome Model Repository

Log in | Register

### Main model listing

The list of processed model exposures (formats: [100 per page](#) | [full list](#)), which are models that have documentation pages generated from the metadata they contain. Alternatively, you may start browsing via the categories that are listed below:

*Please note:* Comments about the functional status or curation status of the models within this repository are the opinions of the CellML Model Repository curators. We do our best to accurately represent these models, but please [contact us](#) if you have a query or issue with comments made on this site.

### CellML models by category

- [Calcium Dynamics](#)
- [Cardiovascular Circulation](#)
- [Cell Cycle](#)
- [Cell Migration](#)
- [Circadian Rhythms](#)
- [Electrophysiology](#)
- [Endocrine](#)
- [Excitation-Contraction Coupling](#)
- [Gene Regulation](#)
- [Immunology](#)
- [Ion Transport](#)
- [Mechanical Constitutive Laws](#)
- [Metabolism](#)
- [Myofilament Mechanics](#)
- [Neurobiology](#)
- [pH Regulation](#)
- [PKPD](#)
- [Signal Transduction](#)
- [Synthetic Biology](#)

### FieldML models

### Searching

Searching of models can be done anywhere on the site using the search box on the upper right hand corner.

Done




Physiome Model Repository — CellML Model Repository - Mozilla Firefox  
FieldML — CellML Model Repository - Mozilla Firefox

File Edit View History Bookmarks Tools Help

http://models.physiomeproject.org/fieldml

Google

FieldML — CellML Model Re... Andre's Hodgkin Huxley mo... PMR2 basic tutorial draft — ...



Search Site

**Models Home** Exposures Workspaces

You are here: [Home](#) → [FieldML](#) [Log in](#) | [Register](#)

## FieldML

This is the beta sample of the FieldML repository. The following is a small list of FieldML models in exnode format which will be converted to FieldML once FieldML 0.2 is released.

- [Laminar structure of the Heart: A mathematical model.](#)
- [Ventricular mechanics in diastole: material parameter sensitivity.](#)

[RSS feed](#) | [Print this](#)

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Done

Physiome Model Repository — CellML Model Repository - Mozilla Firefox  
FieldML — CellML Model Repository - Mozilla Firefox  
Ventricular mechanics in diastole: material parameter sensitivity. — CellML Model Repository - Mozilla Firefox

File Edit View History Bookmarks Tools Help

http://models.physiomeproject.org/exposure/fbe9652676c463daa12e046255

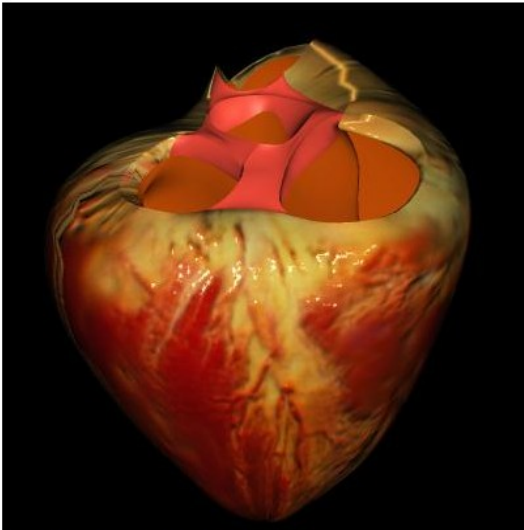
Google

Ventricular mechanics in di... Andre's Hodgkin Huxley mo... PMR2 basic tutorial draft

You are here: [Home](#) → [Exposures](#) → [Ventricular mechanics in diastole: material parameter sensitivity.](#) → Ventricular mechanics in diastole: material parameter sensitivity. [Log in](#) | [Register](#)

## Ventricular mechanics in diastole: material parameter sensitivity.

Models of ventricular mechanics have been developed over the last 20 years to include finite deformation theory, anisotropic and inhomogeneous material properties and an accurate representation of ventricular geometry. As computer performance and the computational efficiency of the models improve, clinical application of these heart mechanics models is becoming feasible. One such application is to estimate myocardial material properties by adjusting the constitutive parameters to match wall deformation from MRI or ultrasound measurements, together with a measurement (or estimate) of ventricular pressure. Pigs are now the principal large animal model for these studies and in this paper we present the development of a new three-dimensional finite element model of the heart based on measurements of the geometry and the fibre and sheet orientations of pig hearts. The end-diastolic deformation of the model is computed using the "pole-zero" constitutive law which we have previously used to model the mechanics of passive myocardial tissue specimens. The sensitivities of end-diastolic fibre-sheet material strains and heart shape to changes in the material parameters are computed for the parameters of the pole-zero law in order to assess the utility of the models for inverse material property determination.



The rendered result of this model.

To launch the model, please select Zinc Viewer under navigation on the right.

### Model Curation

Curation Status: ★★

### Source

Derived from workspace [Per Pixel Lighting at changeset 1d31b32abdd7.](#)

### Downloads

[Complete Archive as .tgz](#)  
[Download This File](#)

### Views available

- [FieldML Metadata](#)
- [Source View](#)
- [Zinc Viewer](#)
- [Cite this model](#)

### License

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### Navigation

- [Ventricular mechanics in diastole: material parameter sensitivity.](#)

Done

Ventricular mechanics in diastole: material parameter sensitivity. — CellML Model Repository - Mozilla Firefox

File Edit View History Bookmarks Tools Help

http://models.physiomeproject.org/exposure/fbe9652676c463daa12e046255

Ventricular mechanics in di... Andre's Hodgkin Huxley mo... PMR2 basic tutorial draft

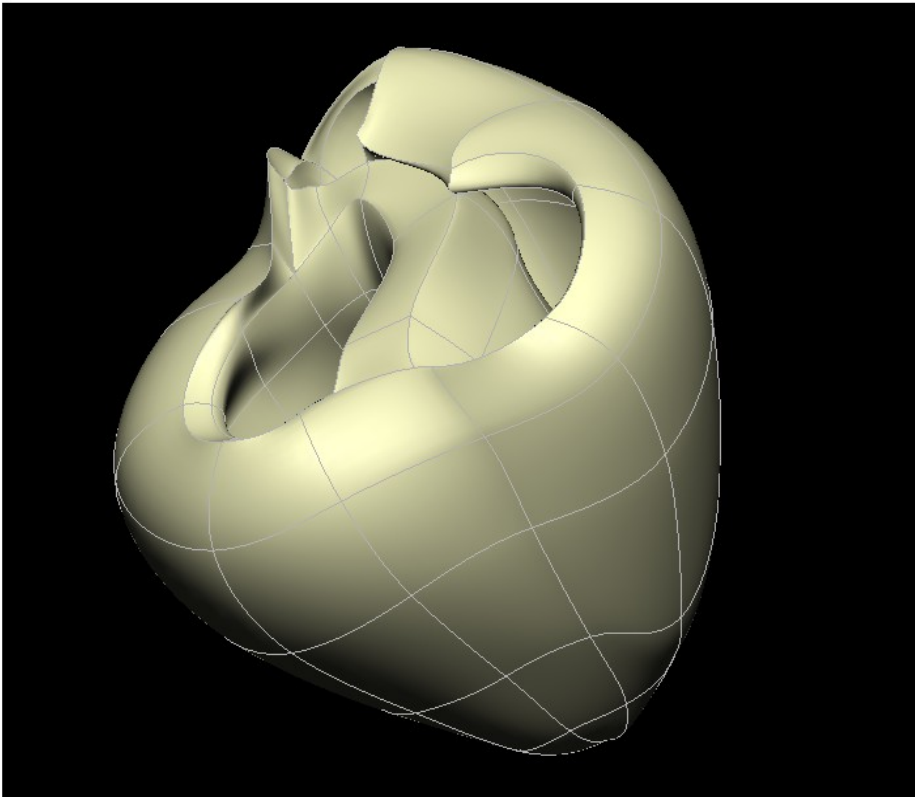
Models Home Exposures Workspaces

You are here: Home → Exposures → Ventricular mechanics in diastole: material parameter sensitivity. → Ventricular mechanics in diastole: material parameter sensitivity. Log in | Register

## Zinc Viewer

The following viewer requires Mozilla Firefox 1.5 to 3.5, and the [Zinc Add-on for Firefox](#) installed.

If you are a user of Firefox 3.6, please see [this page](#) for the add-on.



**Model Curation**  
Curation Status: ★★

**Source**  
Derived from workspace [Per Pixel Lighting](#) at changeset [1d31b32abdd7](#).

**Downloads**  
Complete Archive as .tgz  
[Download This File](#)

**Views available**  
[FieldML Metadata](#)  
[Source View](#)  
[Zinc Viewer](#)  
[Cite this model](#)

**License**  
This work is licensed under a [Creative Commons Attribution 3.0 Unported License](#).

**Navigation**  
[Ventricular mechanics in diastole: material parameter sensitivity.](#)

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Done



**PMR2**  
**The software behind  
the repository**

# Glossary

- Workspace – data agnostic mercurial repository
- Changeset – a representation of a single revision of the content of a workspace
- Exposure – a permanent link to a specific changeset with data rendered for the web
- Exposure plug-ins – an extensible framework for rendering workspace content for web presentation
- Plone CMS – workflow manager; user access controls; web presentation; etc.

# An example from computational physiology

- Build up a multiscale model of the renal nephron
  - ion transporters, cellular models, segmental models, whole nephron...
- Share the various models with collaborators
- Publish the model along the way
  
- Disclaimer: not all the following features are implemented/integrated in either language specifications and/or supporting software tools – and such features may change considerably before they are supported.

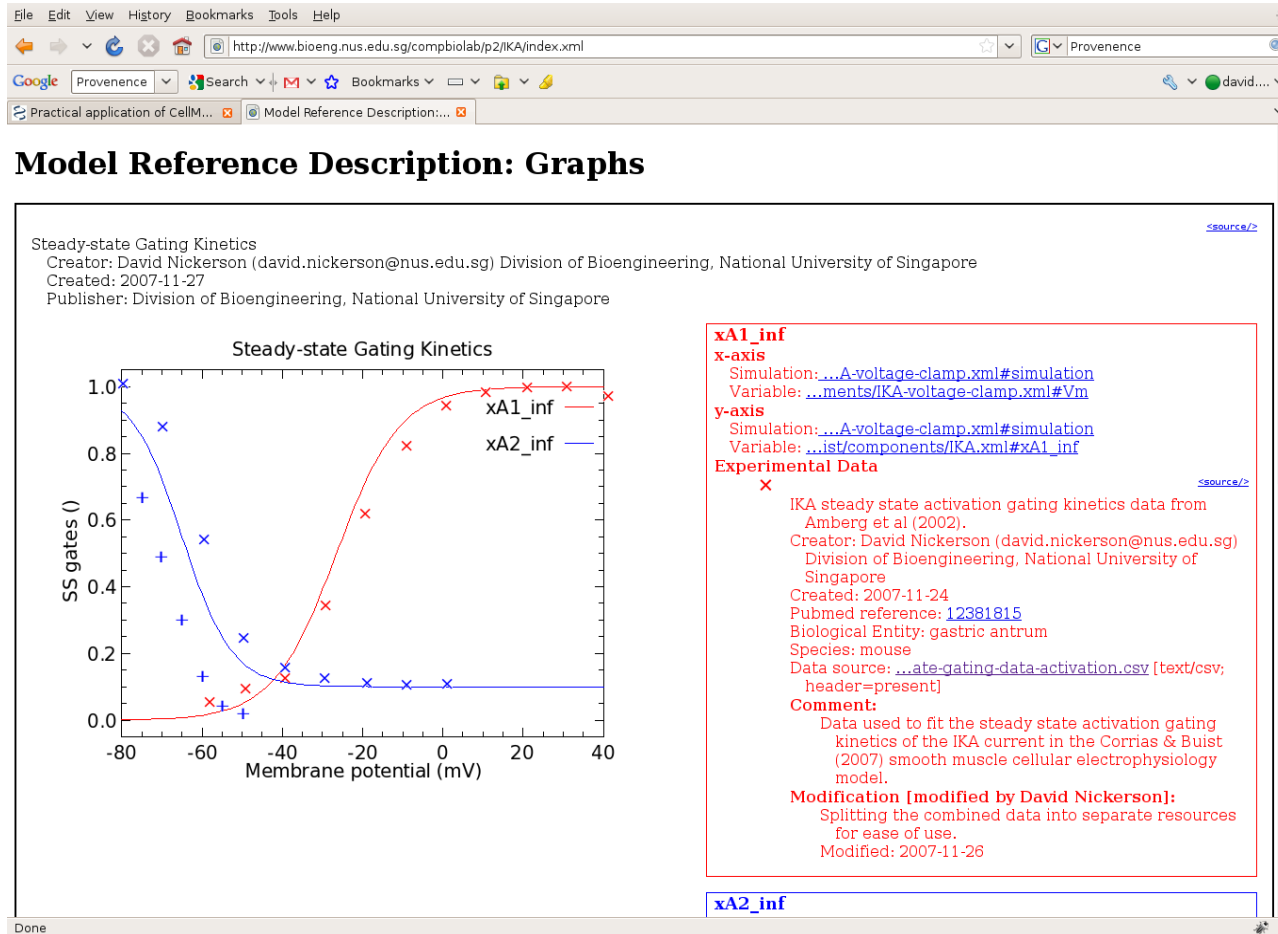
# Membrane transporters



(Workspace)



# Membrane transporters



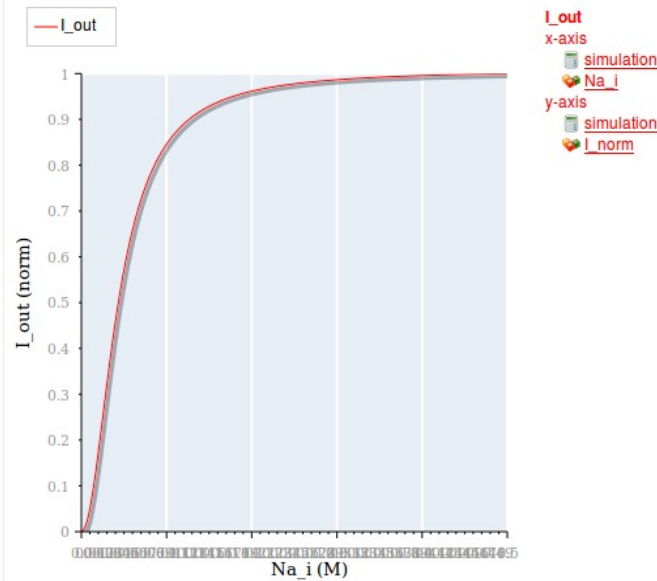


### Constituents of the Renal Nephron

David Nickerson (2010-04-19)

- Constituents of the Renal Nephron
  - Eskandari et al (2005)
    - Figure 2(b)
    - Figure 3(a)
    - Figure 3(b)
  - Figure 4
  - Mackenzie et al (1996)
    - Figure 3(a)
    - Figure 3(b)
    - Figure 3(c)
    - Figure 3(d)

Reproduction of figure 4 from Eskandari et al (2005).



#### I\_norm

Units: dimensionless

Defined in math container:  $\sqrt{Na_i}$

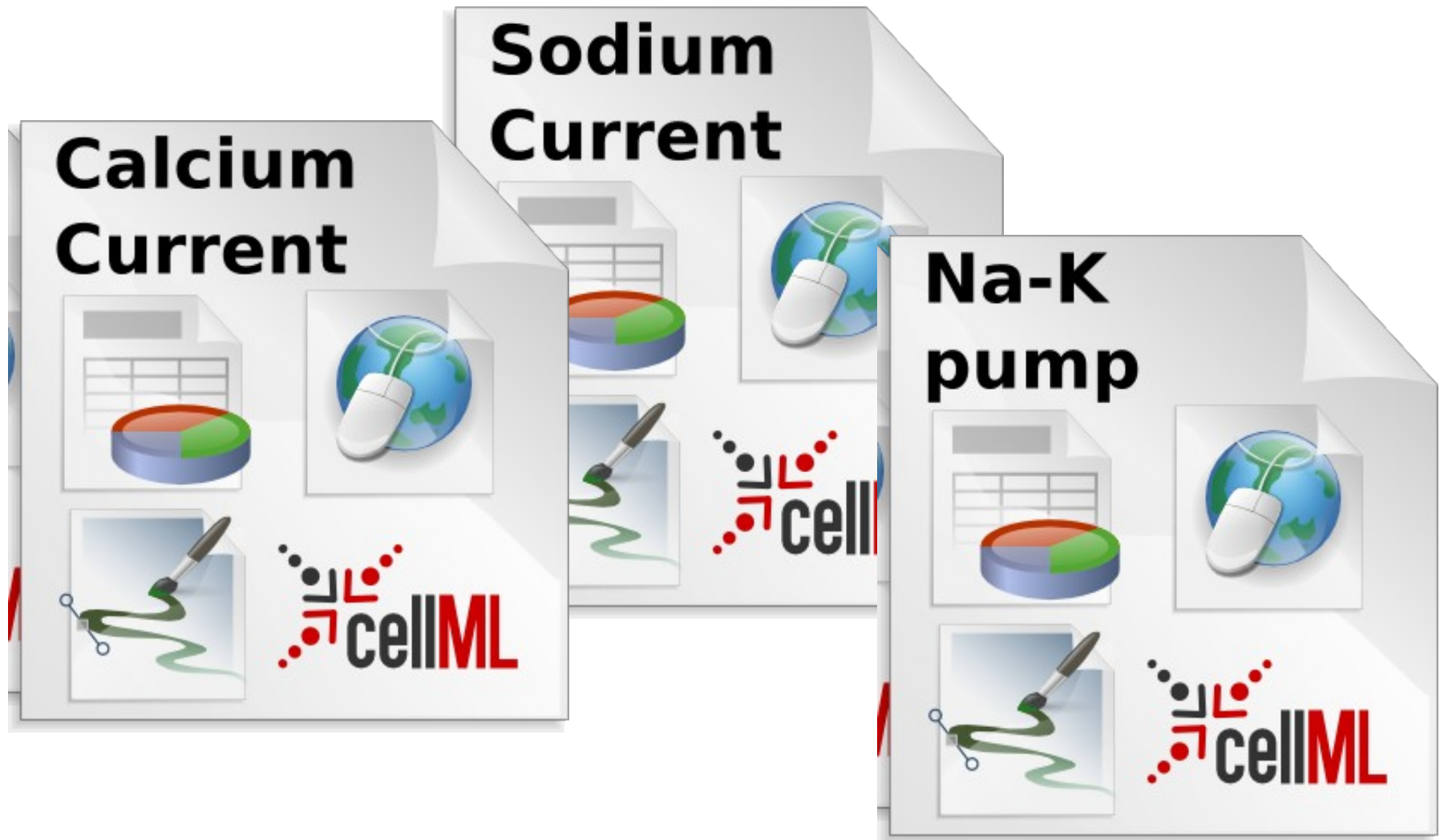
#### Na\_i

+ Created: 2010-04-21, David Nickerson

$$\frac{dNa_i}{dtime} = [1.0e-3M\_per\_second]$$

$$I\_norm = \sqrt{Na_i} / [6.29510065e-06uA]$$

# Membrane transporters



# Assemble a cell model

## Epithelial Cell

### Sodium Current

### Calcium Current

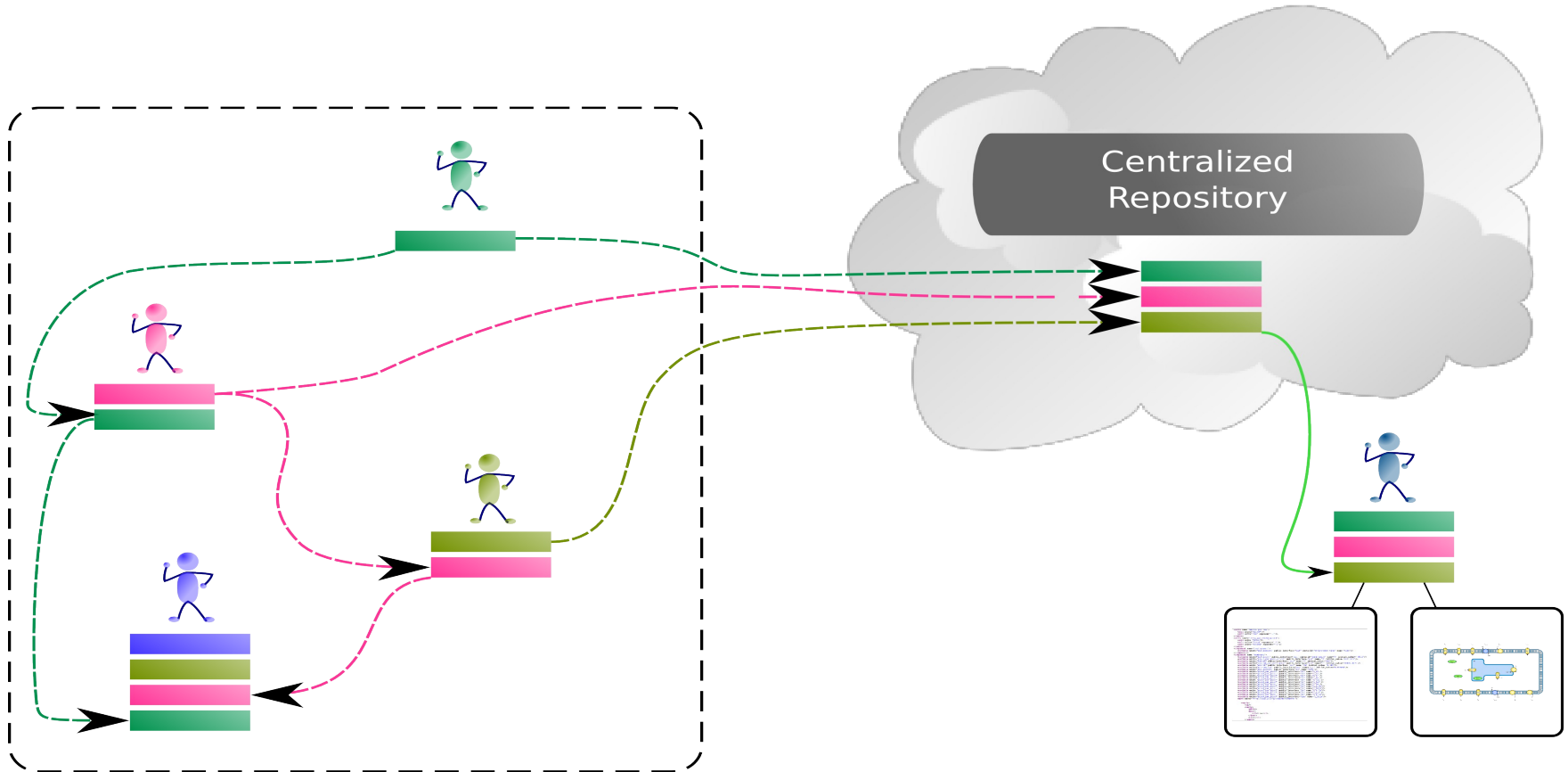
### Na-K pump



# Embedded workspaces

- Intended to manage the separation of modules which are integrated to create a model
- Facilitate the sharing and reuse of model components independently from the source model
- Enables the development of the modules to proceed independently, thus the version of the workspaces embedded is also tracked
- Allows authors to make use of relative URIs when linking data resources providing a file system agnostic method to describe complex module relationships in a portable manner

# Collaborative model development



# Versioning embedded workspaces

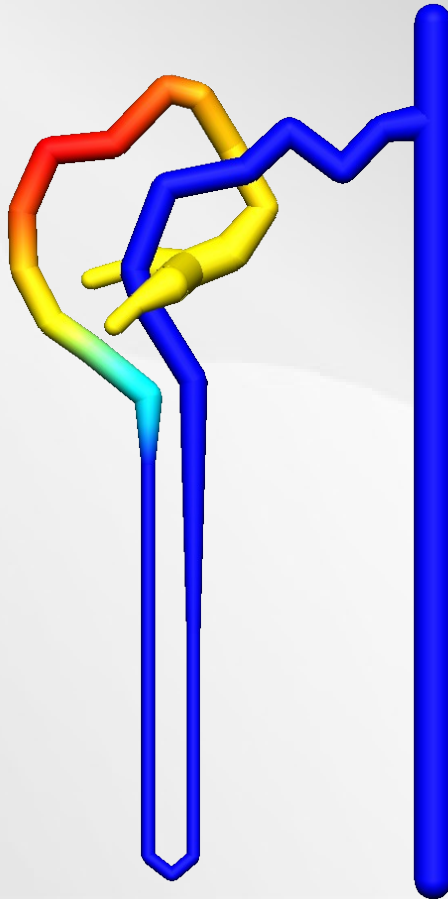
- Workspaces can be embedded at a specific revision or set to track the most recent revision of the source workspace
- Changes made to the source workspace will not affect the embedding workspace until the author explicitly chooses to update the embedded workspace
- Provides the author with the opportunity to review the changesets and make an informed decision regarding alterations to embedded revisions

# Data agnostic workspaces

- Generic mercurial repositories
- Can contain any format data (currently relatively unrestricted)
  - CellML, SBML, FieldML, SED-ML, PDF, .doc, ...
- No restriction to models only
  - experimental data, simulation results, generated images, ...

# Multiscale models

## Renal Nephron

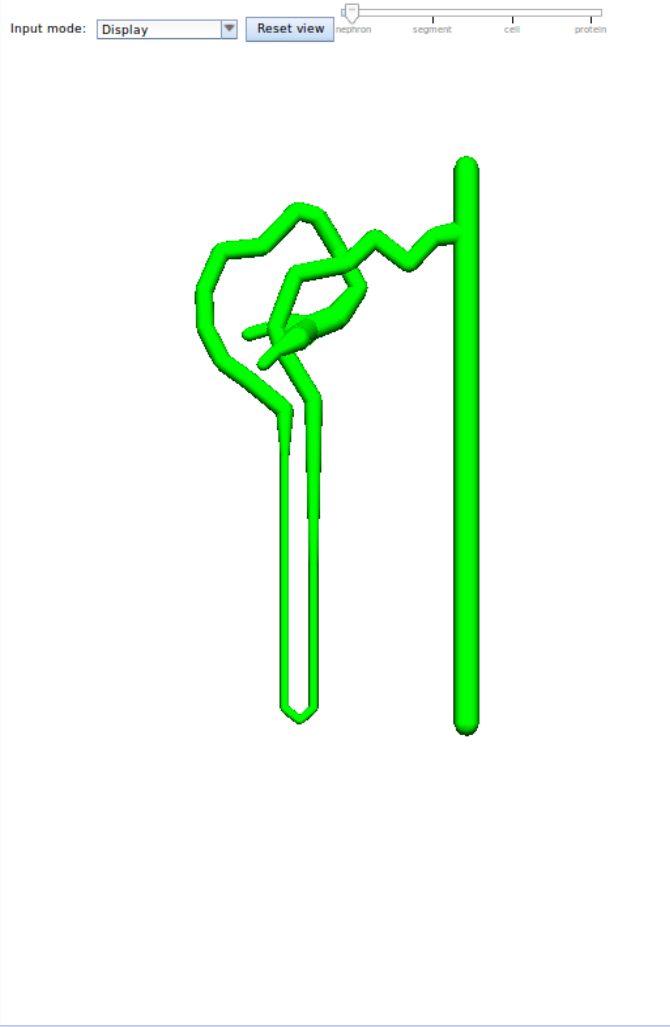




# The Renal Nephron

Close all

- Nephron
  - Anatomy
    - Efferent Arteriole
    - Afferent Arteriole
    - Glomerulus
    - Proximal Tubule
      - Proximal Convoluted Tu
      - Proximal Straight Tubul
    - Loop of Henle
      - Macula Densa
      - Distal Convoluted Tubule
      - Connecting Tubule
      - Collecting Duct
  - Physiology
    - Efferent Arteriole
    - Afferent Arteriole
    - Glomerulus
    - Proximal Tubule
      - Weinstein et al (2007)
      - Thomas and Dagher (19
    - Loop of Henle
      - Macula Densa
    - Distal Convoluted Tubule
    - Connecting Tubule
    - Collecting Duct
  - Modelling Studies
    - SGLT2 Inhibition
      - Na-glucose cotransport
      - Control
      - Inhibited



## Nephron

A demonstration renal nephron model interface.

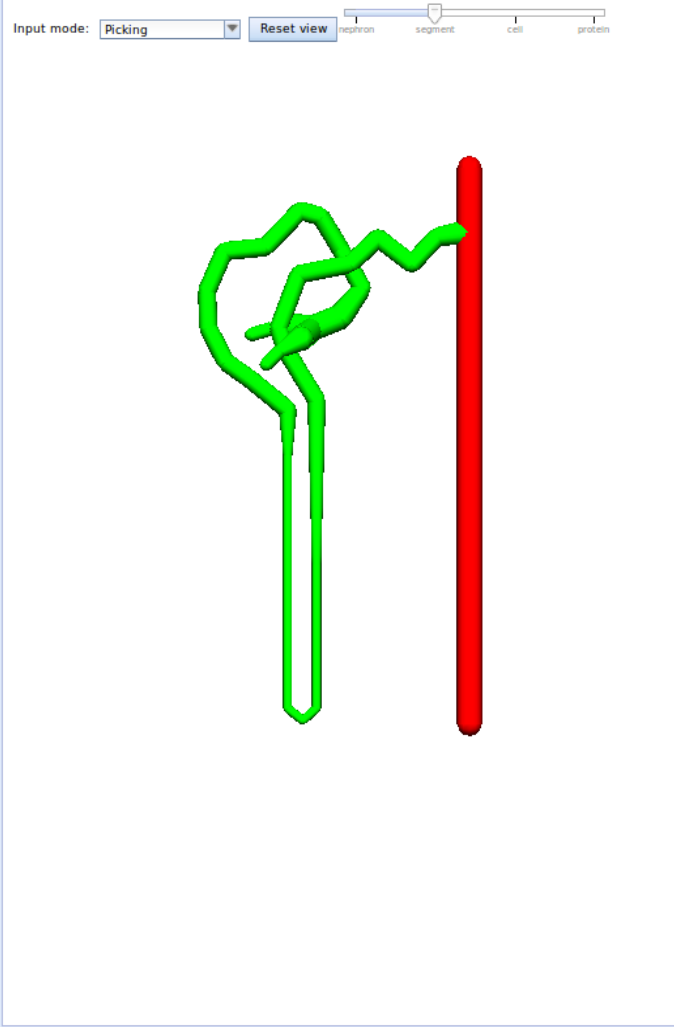
This prototype interface provides the user with an anatomical browser, cellular and subcellular transport model database, and some preliminary simulation results for your viewing pleasure. The tree on the left hand side provides the primary overview of the content of this interface, the central pane provides the graphical view where relevant, and this pane shows the details.



# The Renal Nephron

Close all

- Nephron
  - Anatomy
    - Efferent Arteriole
    - Afferent Arteriole
    - Glomerulus
    - Proximal Tubule
      - Proximal Convoluted Tu
      - Proximal Straight Tubul
    - Loop of Henle
      - Macula Densa
      - Distal Convoluted Tubule
      - Connecting Tubule
      - Collecting Duct**
  - Physiology
    - Efferent Arteriole
    - Afferent Arteriole
    - Glomerulus
    - Proximal Tubule
      - Weinstein et al (2007)
      - Thomas and Dagher (15
    - Loop of Henle
      - Macula Densa
    - Distal Convoluted Tubule
    - Connecting Tubule
    - Collecting Duct
  - Modelling Studies
    - SGLT2 Inhibition
      - Na-glucose cotransport
      - Control
      - Inhibited



## Collecting Duct

The tubules and ducts that link the nephron tubule with the ureter.

The nephron tubule empties into the collecting duct system, which begins in the medullary ray of the cortex and descends along the axis of the nephron, through the medulla, before draining into a papillary duct. The collecting ducts play a significant role in the 'fine-tuning' of electrolyte and water balance through the hormonal regulation of the permeability of these segments.

In the human cortex, approximately 11 nephron tubules merge into a single cortical collecting duct. As it descends through the medulla, the collecting ducts merge on average about 8 times before draining into the papillary duct.

Related CellML models:

- [Weinstein \(2002\)](#)

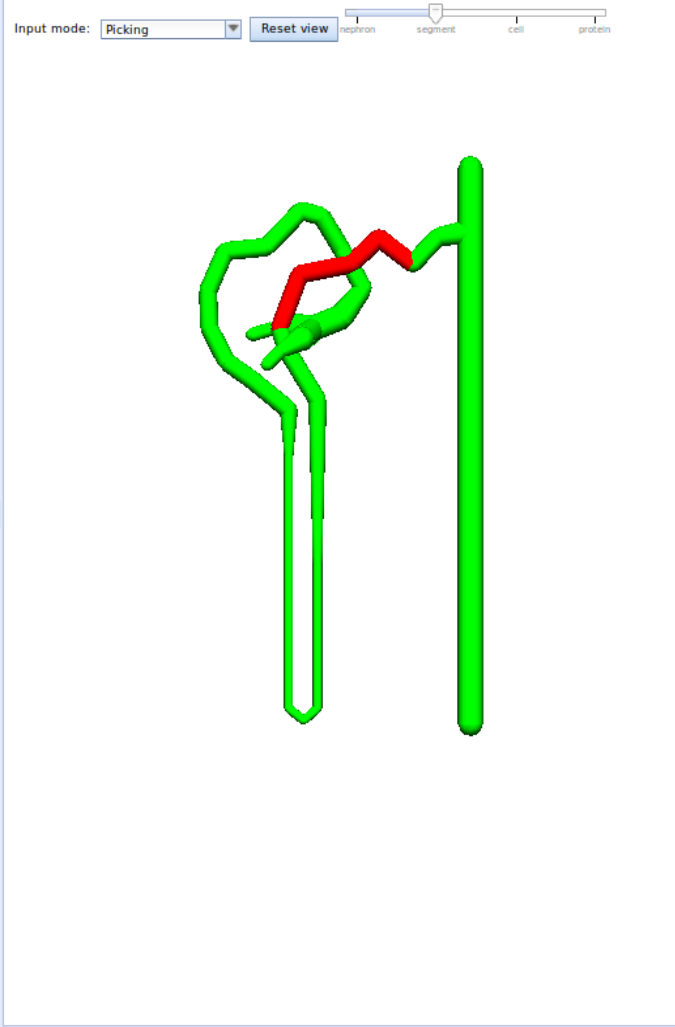
## Distal Convoluted Tubule

The segment of tubule between the thick ascending limb and the collecting ducts.

## The Renal Nephron

Close all

- Nephron
  - Anatomy
    - Efferent Arteriole
    - Afferent Arteriole
    - Glomerulus
    - Proximal Tubule
      - Proximal Convoluted Tu
      - Proximal Straight Tubul
    - Loop of Henle
      - Macula Densa
      - Distal Convoluted Tubule**
      - Connecting Tubule
      - Collecting Duct
  - Physiology
    - Efferent Arteriole
    - Afferent Arteriole
    - Glomerulus
    - Proximal Tubule
      - Weinstein et al (2007)
      - Thomas and Dagher (19
    - Loop of Henle
      - Macula Densa
      - Distal Convoluted Tubule
      - Connecting Tubule
      - Collecting Duct
  - Modelling Studies
    - SGLT2 Inhibition
      - Na-glucose cotransport
      - Control
      - Inhibited



### Distal Convoluted Tubule

The segment of tubule between the thick ascending limb and the collecting ducts.

Sometimes referred to as the early distal tubule. The distal convoluted tubule is located in the cortex where, as per the proximal convoluted tubule, it has a convoluted trajectory through the tissue. The permeability of the distal convoluted tubule resembles that of the thick ascending limb - i.e. virtually impermeable to water and urea but permeable to salt and other electrolytes. Thus as these solutes are reabsorbed, the luminal fluid becomes increasing dilute. This segment is involved in the hormonal regulation of K, Na, Ca and pH.

Related CellML models:

- [Weinstein et al \(2005\)a](#)
- [Chang & Fujita \(1999\)](#)
- [Chang and Fujita \(2001\)](#)

### Nephron

A demonstration renal nephron model interface.

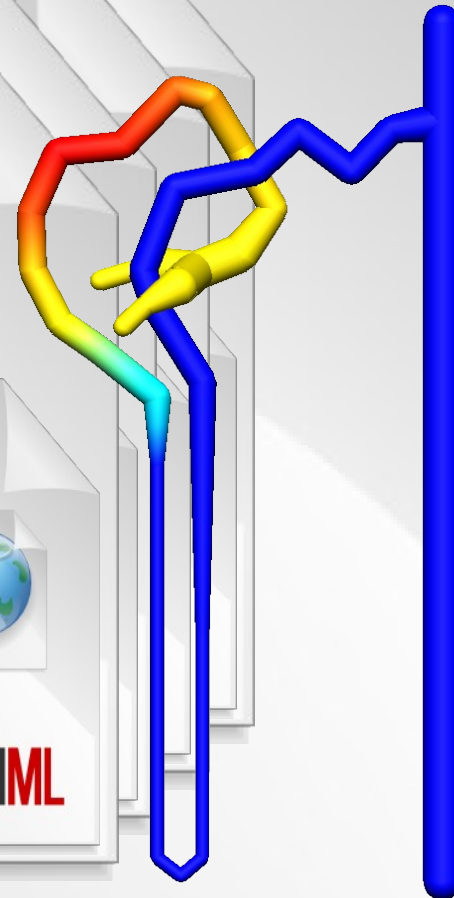
# Renal Nephron

Epithelial Cell

Sodium  
Current

Calcium  
Current

Na-K  
pump

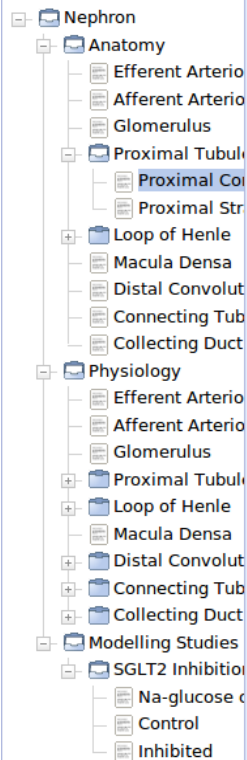


CellML icons and logos

The image shows a collection of icons and logos associated with CellML. It includes a 3D pie chart, a computer mouse, a globe with a plant, a calculator, a document with a green line graph, and the CellML logo (a stylized 'L' with dots) and the text 'cellML'.

## The Renal Nephron

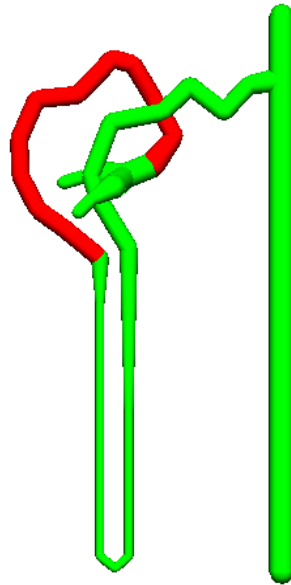
Close all



Input mode: Picking

Reset view

nephron segment cell protein



## Proximal Tubule

First of the transporting tubule segments.

From the Bowman's Capsule, the filtered fluid enters the first of the reabsorptive epithelial tubule segments - the proximal tubule. The proximal tubule consists of a convoluted portion and a straight portion. This segment has a high transport activity and is responsible for the bulk of the salt and water reabsorption. Furthermore, the majority of the key organic molecules (glucose and amino acids), as well as other important ions (K, Ca, HCO<sub>3</sub>), are actively reabsorbed in this segment.

Related CellML models:

- [Weinstein et al \(2007\)](#)
- [Thomas and Dagher \(1994\)](#)

## Proximal Convoluted Tubule

Convoluted portion of the Proximal Tubule.

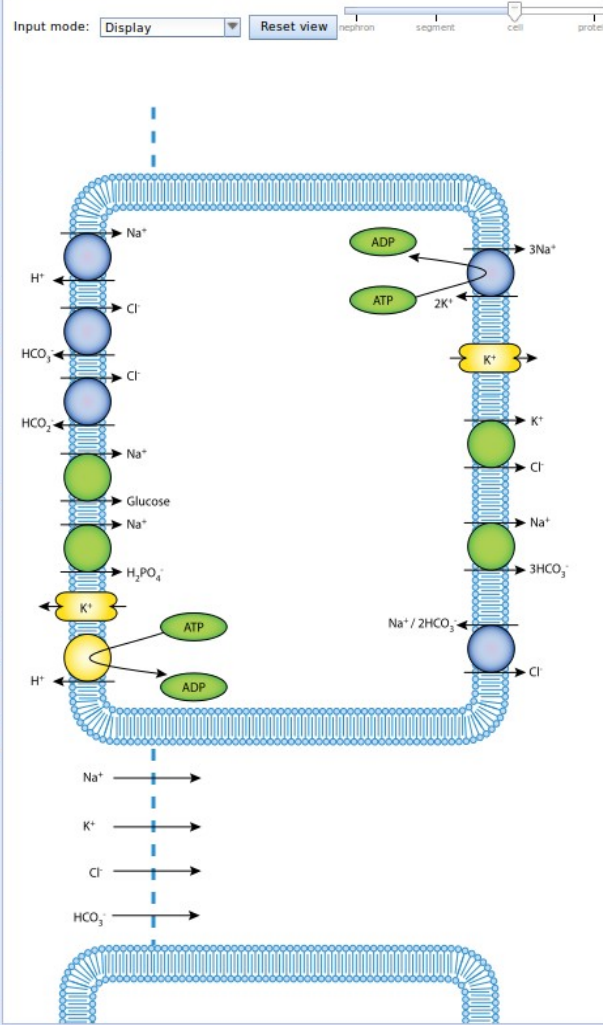
As its name suggests, the proximal convoluted tubule undergoes a convoluted trajectory through the cortical region of the kidney, primarily the cortical labyrinth.



# The Renal Nephron

Close all

- Nephron
  - Anatomy
    - Efferent Arterio
    - Afferent Arterio
    - Glomerulus
    - Proximal Tubul
      - Proximal Co
      - Proximal Str
  - Loop of Henle
  - Macula Densa
  - Distal Convolut
  - Connecting Tub
  - Collecting Duct
  - Physiology
    - Efferent Arterio
    - Afferent Arterio
    - Glomerulus
    - Proximal Tubul
      - Weinstein et
      - Thomas and
    - Loop of Henle
    - Macula Densa
    - Distal Convolut
    - Connecting Tub
    - Collecting Duct
  - Modelling Studies
    - SGLT2 Inhibitio
    - Na-glucose c
    - Control
    - Inhibited

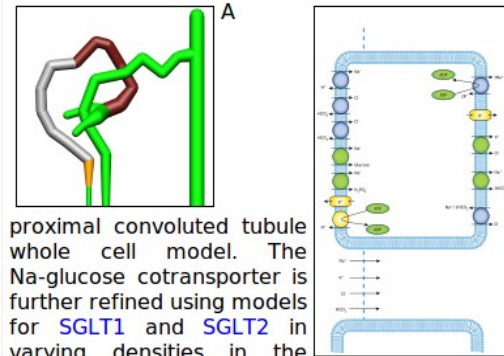


Related CellML models:

- [Weinstein et al \(2007\)](#)
- [Thomas and Dagher \(1994\)](#)

## Weinstein et al (2007)

[Flow-dependent transport in a mathematical model of rat proximal tubule.](#) *Am J Physiol Renal Physiol* **292**: F1164-F1181, 2007.



proximal convoluted tubule whole cell model. The Na-glucose cotransporter is further refined using models for SGLT1 and SGLT2 in varying densities in the different segments of the proximal tubule.

## Proximal Convoluted Tubule

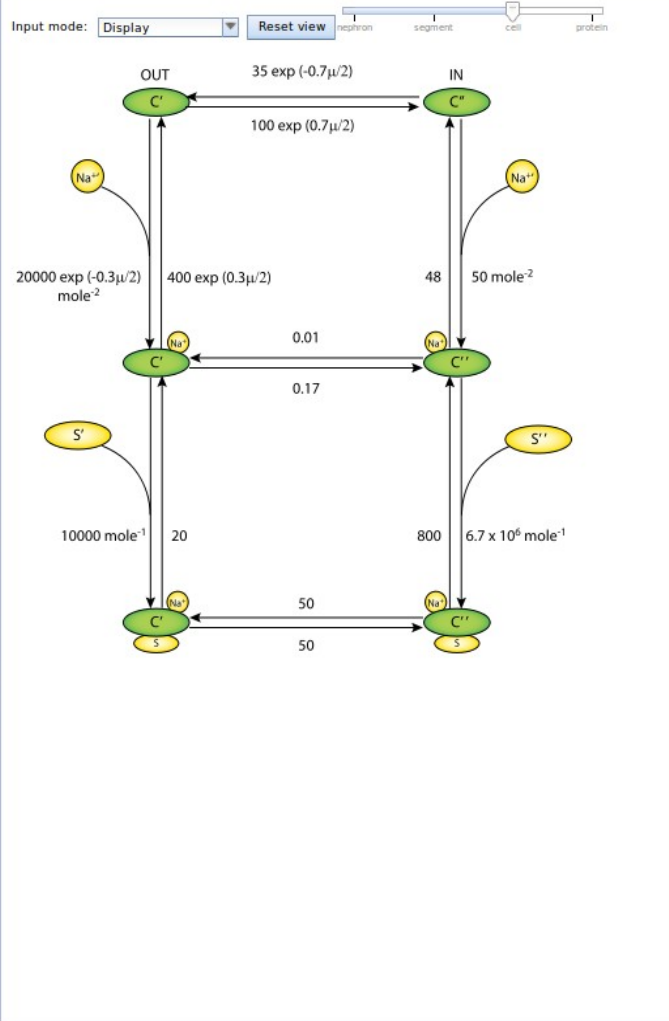
Convoluted portion of the Proximal Tubule.



# The Renal Nephron

Close all

- Nephron
  - Anatomy
    - Efferent Arterio
    - Afferent Arterio
    - Glomerulus
    - Proximal Tubul
    - Proximal Co
    - Proximal Str
  - Loop of Henle
  - Macula Densa
  - Distal Convolut
  - Connecting Tub
  - Collecting Duct
- Physiology
  - Efferent Arterio
  - Afferent Arterio
  - Glomerulus
  - Proximal Tubul
  - Weinstein et
  - Thomas and
  - Loop of Henle
  - Macula Densa
  - Distal Convolut
  - Connecting Tub
  - Collecting Duct
- Modelling Studies
  - SGLT2 Inhibition
    - Na-glucose c
    - Control
    - Inhibited



## Na-glucose cotransporter

Refined Na-glucose cotransporter models, [SGLT1](#) and [SGLT2](#).

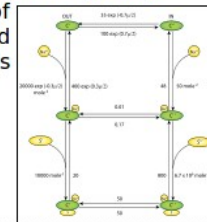
In this study, we utilize the [Weinstein et al \(2007\)](#) proximal tubule model extended through the inclusion of a spatial distribution of the [SGLT1](#) and [SGLT2](#) Na-glucose cotransporter models.

## Mackenzie et al (1996)

[Biophysical Characteristics of the Pig Kidney Na<sup>+</sup>/Glucose Cotransporter SGLT2 Reveal a Common Mechanism for SGLT1 and SGLT2.](#) *J Biol Chem* **271**: 32678-32683, 1996.

[CellML model repository](#)

A complete description of this model is [available](#) and will be intergrated into this interface as future work.



## Proximal Tubule

First of the transporting tubule segments.



## Constituents of the Renal Nephron

David Nickerson (2010-04-19)

[Help](#)

- Constituents of the Renal Nephron
  - Eskandari et al (2005)
    - Eskandari et al (2005)
      - Figure 2(b)
    - Eskandari et al (2005)
      - Figure 3(a)
      - Figure 3(b)
    - Eskandari et al (2005)
      - Figure 4
  - Mackenzie et al (1996)
    - Figure 3(a)
    - Figure 3(b)
    - Figure 3(c)
    - Figure 3(d)

### Constituents of the Renal Nephron

+ S Eskandari *et al* (2005) + 2 more...

+ Last modified: 2010-04-21, David Nickerson (Created: 2010-04-19, David Nickerson)

This reference description is attempting to document, validate, and collect models in the CellML model repository which are relevant to the renal nephron. As the whole nephron model is built this collection will grow.

We are actively developing a whole nephron model and will use this workspace in the CellML model repository to collect all relevant models. As appropriate, the model validation studies and application will also be described here.

#### Tasks:

- [Eskandari et al \(2005\)](#)
- [Mackenzie et al \(1996\)](#)



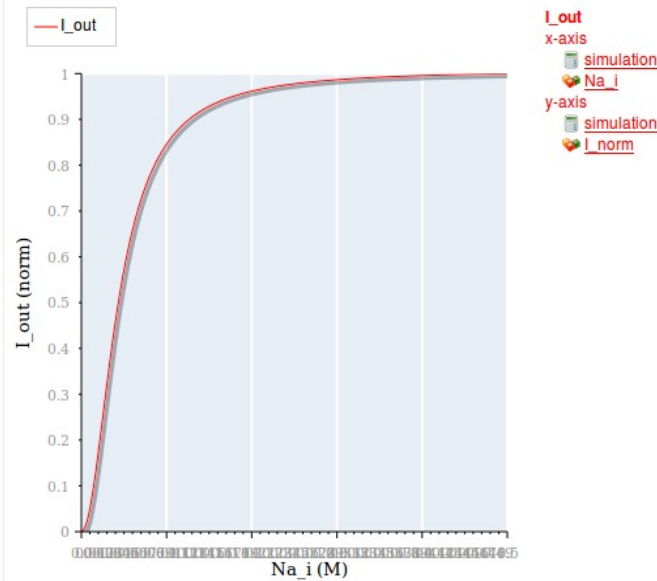


### Constituents of the Renal Nephron

David Nickerson (2010-04-19)

- Constituents of the Renal Nephron
  - Eskandari et al (2005)
    - Figure 2(b)
    - Figure 3(a)
    - Figure 3(b)
  - Figure 4
  - Mackenzie et al (1996)
    - Figure 3(a)
    - Figure 3(b)
    - Figure 3(c)
    - Figure 3(d)

Reproduction of figure 4 from Eskandari et al (2005).



#### I\_norm

Units: dimensionless

Defined in math container:  $\sqrt{Na_i}$

#### Na\_i

+ Created: 2010-04-21, David Nickerson

$$\frac{dNa_i}{dtime} = [1.0e-3M\_per\_second]$$

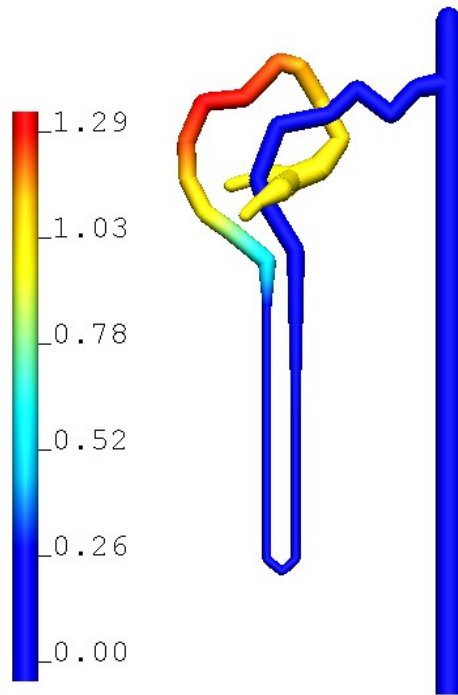
$$I\_norm = \sqrt{Na_i} / [6.29510065e-06uA]$$

# The Renal Nephron

Close all

- Nephron
  - Anatomy
  - Physiology
  - Modelling Studies
    - SGLT2 Inhibition
      - Na-glucose cotransporter
      - Control
      - Inhibited

Input mode: Display Reset view



## Inhibited

The altered glucose concentration observed when SGLT2 is inhibited.

These results show the altered glucose concentration in the proximal tubule when the control SGLT2 mode is inhibited, as would be the case if the drug dapagliflozin was applied to inhibit SGLT2 activity.

## Na-glucose cotransporter

Refined Na-glucose cotransporter models, SGLT1 and SGLT2.

In this study, we utilize the Weinstein et al (2007) proximal tubule model extended through the inclusion of a spatial distribution of the SGLT1 and SGLT2 Na-glucose cotransporter models.

## SGLT2 Inhibition

The selective inhibition of the Na-glucose cotransporter, SGLT2, by the drug Dapagliflozin.

Inhibition of SGLT2 is emerging as an effective treatment of type 2 diabetes. The drug

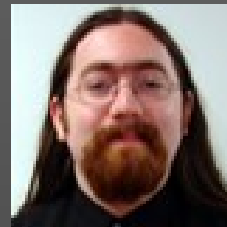


# OpenCMISS

- Connecting variables in CellML models to field components in a finite element model
  - Prototype for linking CellML and FieldML models?
- Allows information to flow in both directions
  - Field values can be controlled by the CellML model and CellML model variables can be controlled by field components
- Will have the ability to make use of many different CellML models which can be simulated independently
- Each CellML model may be replicated many millions of times for large scale problems
  - Distributed computing, GPUs, FPGAs, ...

# Acknowledgements

## “Team CellML”



# Acknowledgements

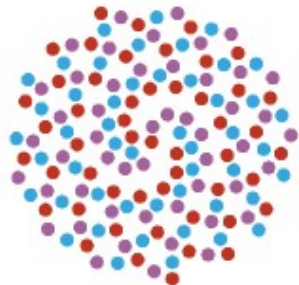


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